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Rowe et al.

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(54) **DEVICES AND METHODS FOR REDUCING CARDIAC VALVE REGURGITATION**

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(65) **Prior Publication Data**

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Related U.S. Application Data

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(51) **Int. Cl.**
A61F 2/24 (2006.01)

(52) **U.S. Cl.**
CPC **A61F 2/2427** (2013.01); **A61F 2/246** (2013.01); **A61F 2/2454** (2013.01); **A61F 2/2463** (2013.01); **A61F 2/2466** (2013.01); **A61F 2/2424** (2013.01); **A61F 2210/0061** (2013.01);

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(58) **Field of Classification Search**

CPC .. **A61F 2/2427**; **A61F 2/2454**; **A61F 2/2463**;
A61F 2/2466

See application file for complete search history.

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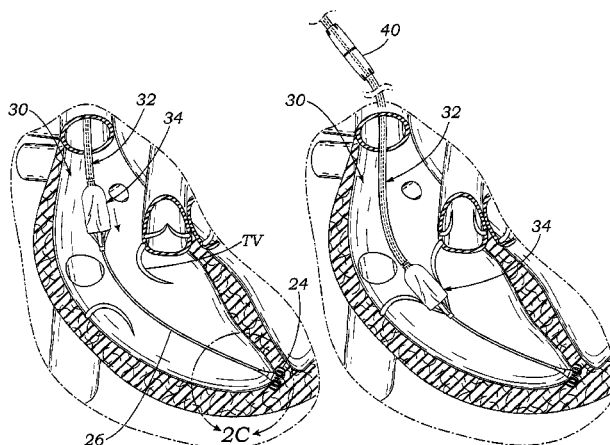
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(57) **ABSTRACT**

The present invention relates to devices and methods for improving the function of a defective heart valve, and particularly for reducing regurgitation through an atrioventricular heart valve—i.e., the mitral valve and the tricuspid valve. For a tricuspid repair, the device includes an anchor deployed in the tissue of the right ventricle, in an orifice opening to the right atrium, or anchored to the tricuspid valve. A flexible anchor rail connects to the anchor and a coaptation element on a catheter rides over the anchor rail. The catheter attaches to the proximal end of the coaptation element, and a locking mechanism fixes the position of the coaptation element relative to the anchor rail. Finally, there is a proximal anchoring feature to fix the proximal end of the coaptation catheter subcutaneously adjacent the subclavian vein. The coaptation element includes an inert covering and helps reduce regurgitation through contact with the valve leaflets.

21 Claims, 31 Drawing Sheets



(52) **U.S. CL.**

CPC .. *A61F2230/0023* (2013.01); *A61F 2250/001*
(2013.01); *A61F 2250/0003* (2013.01)

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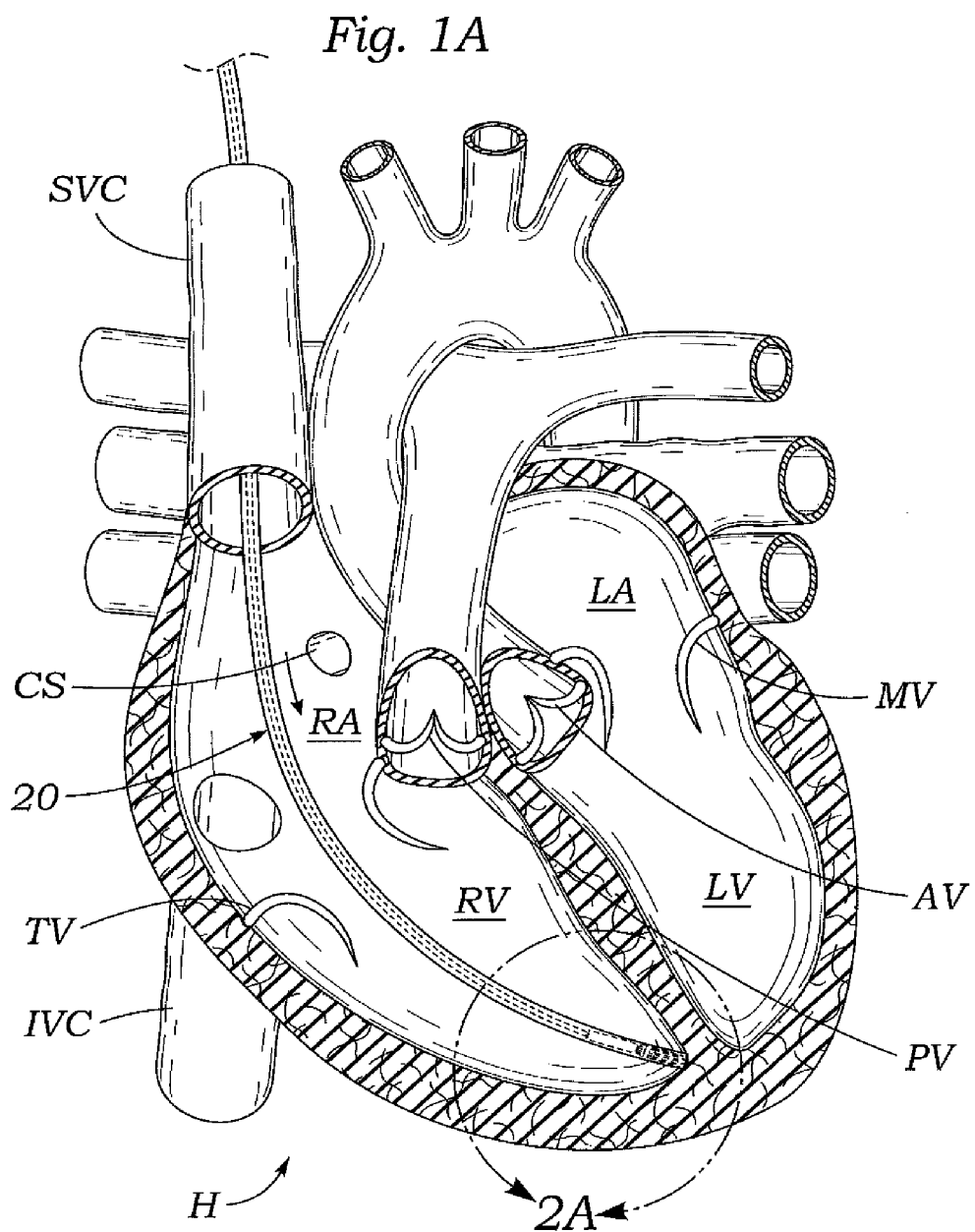
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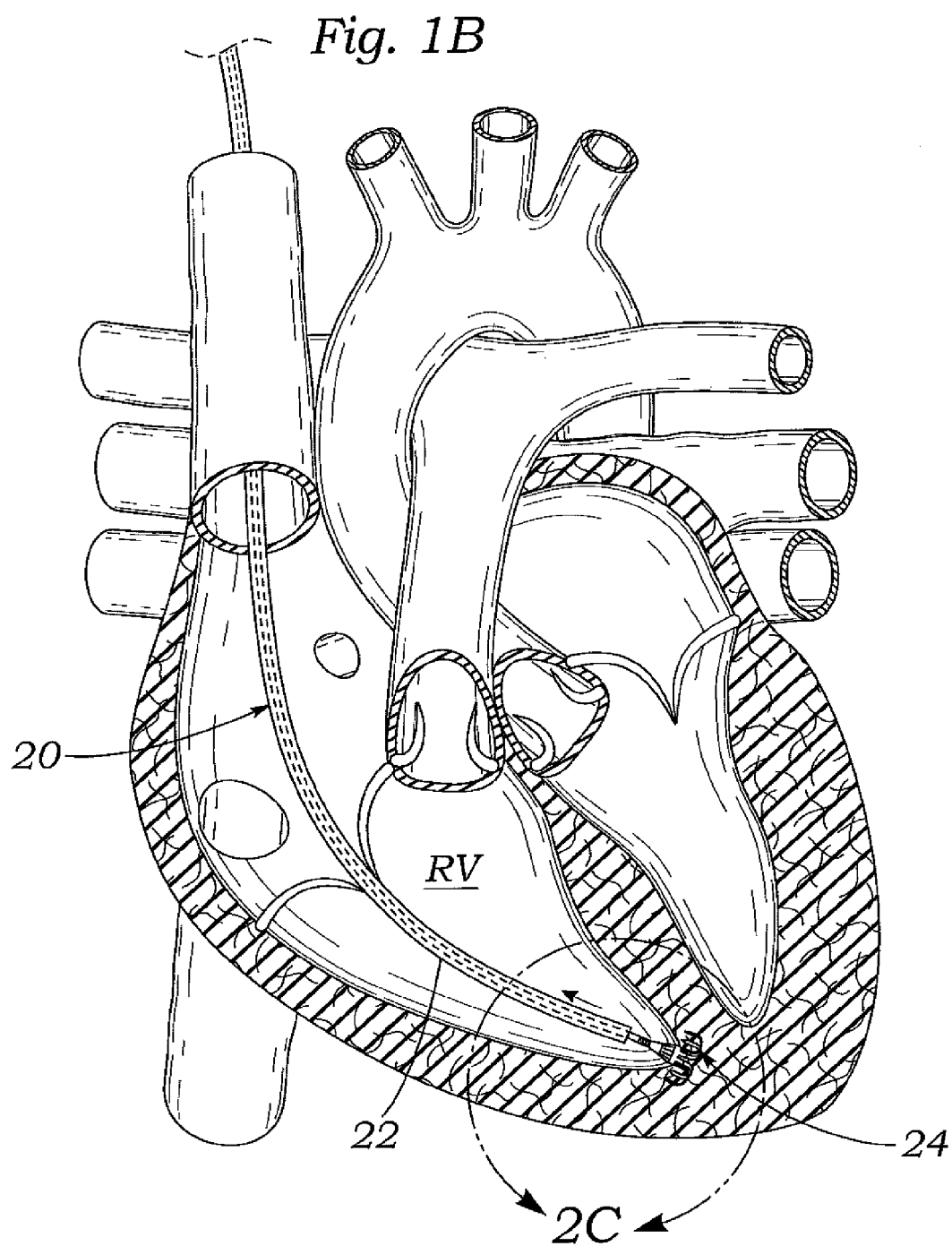


Fig. 2A

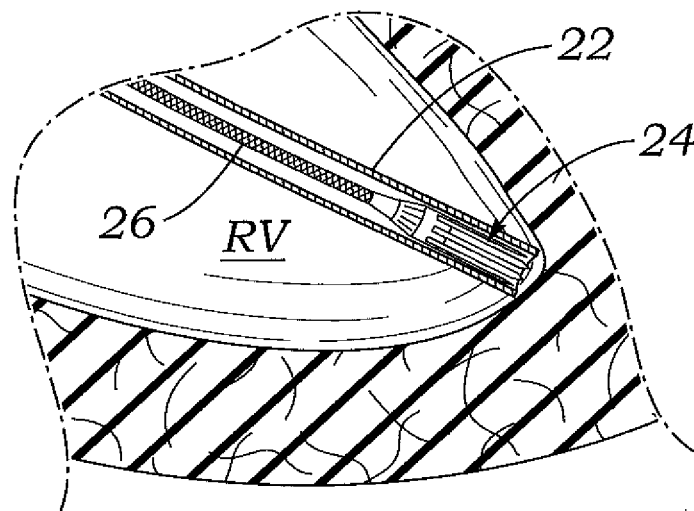


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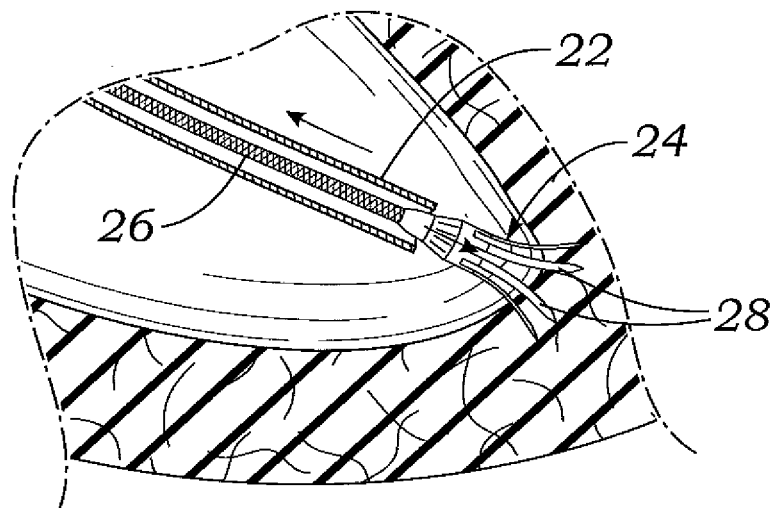
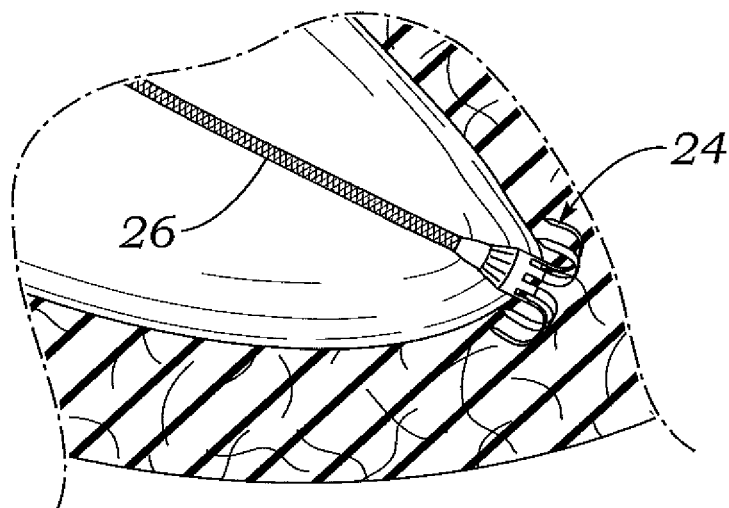
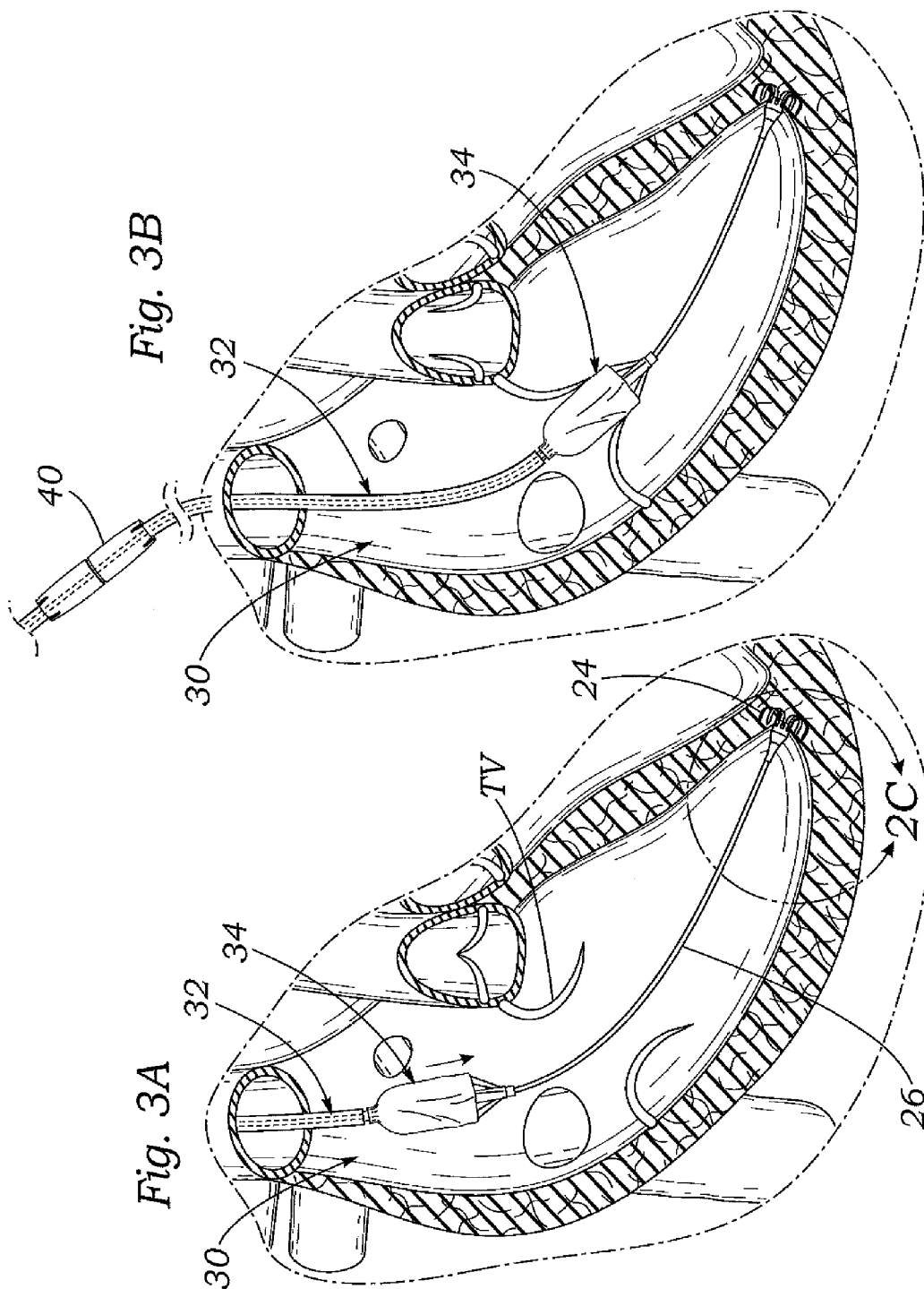
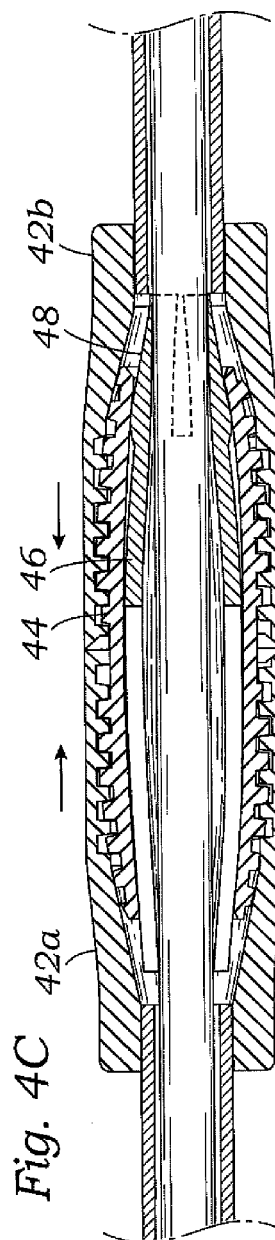
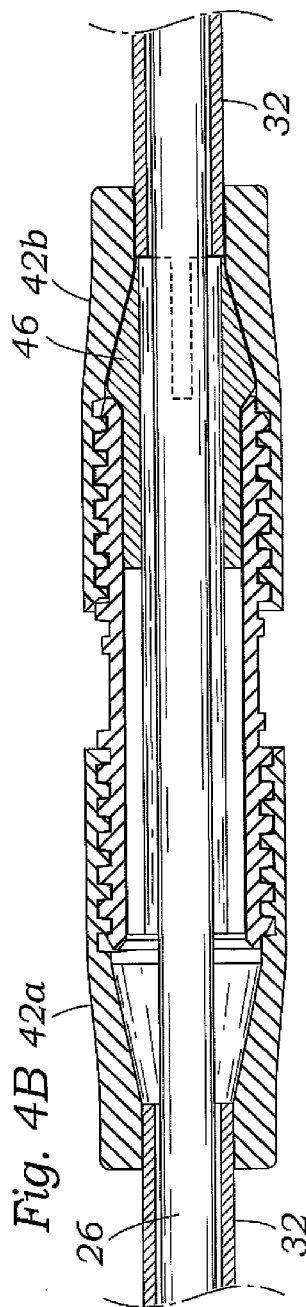
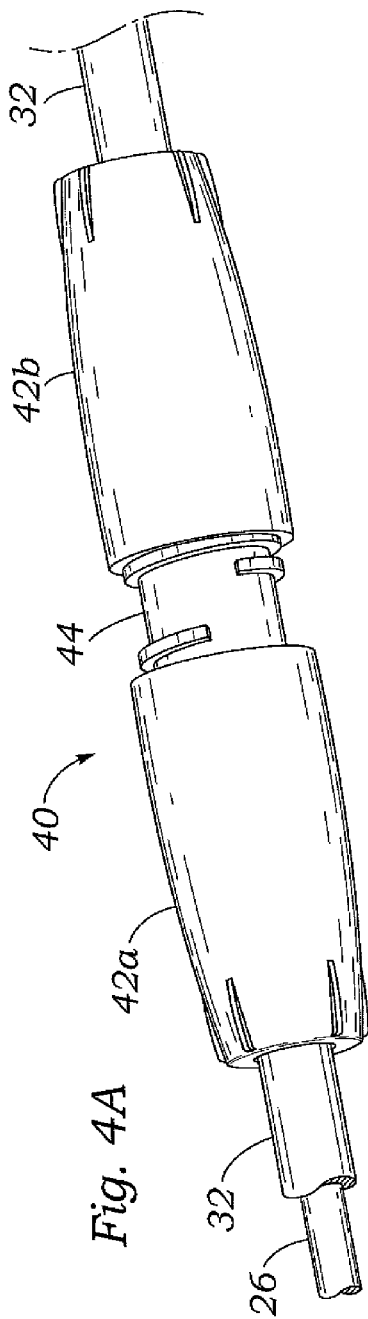
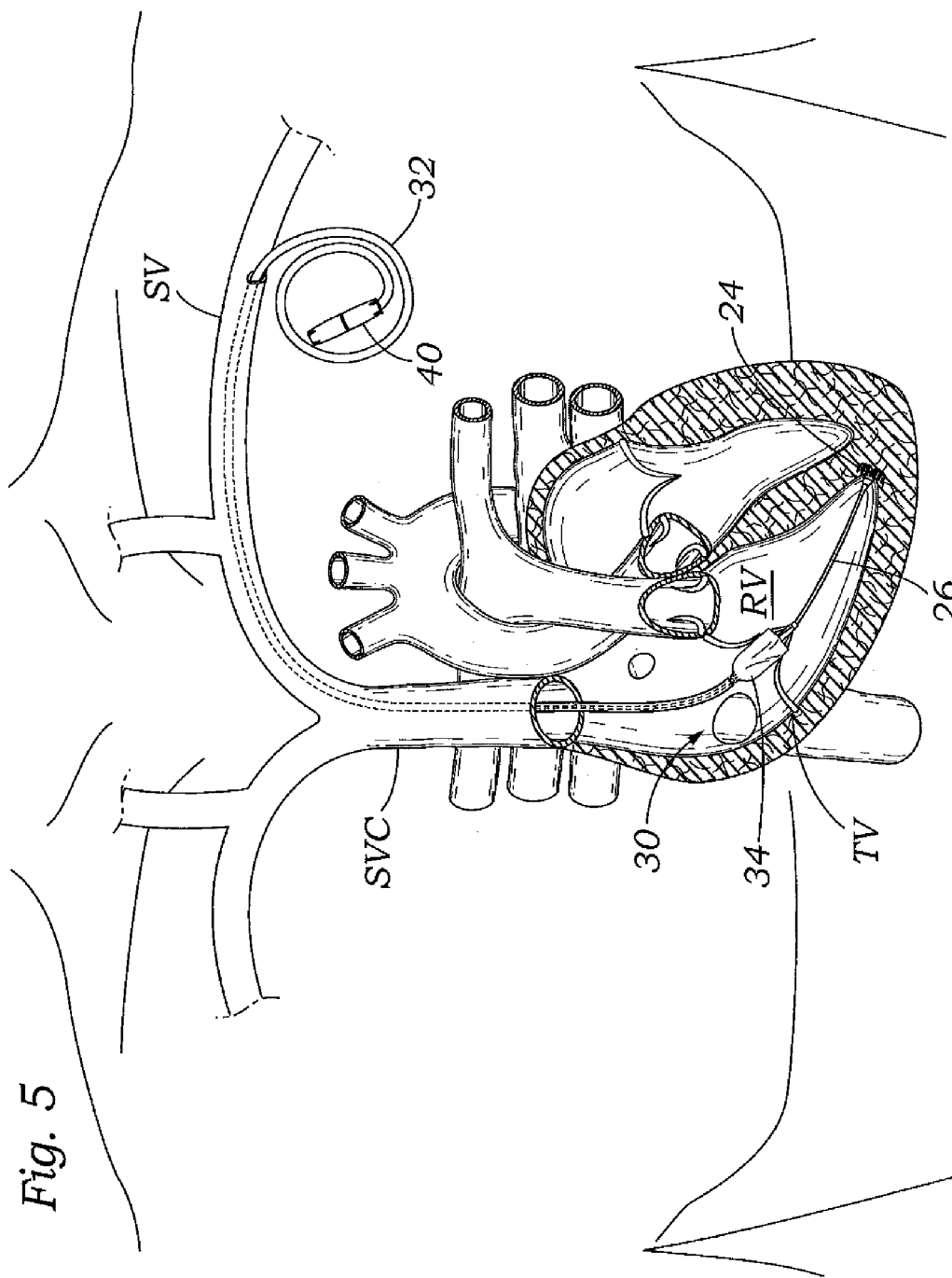


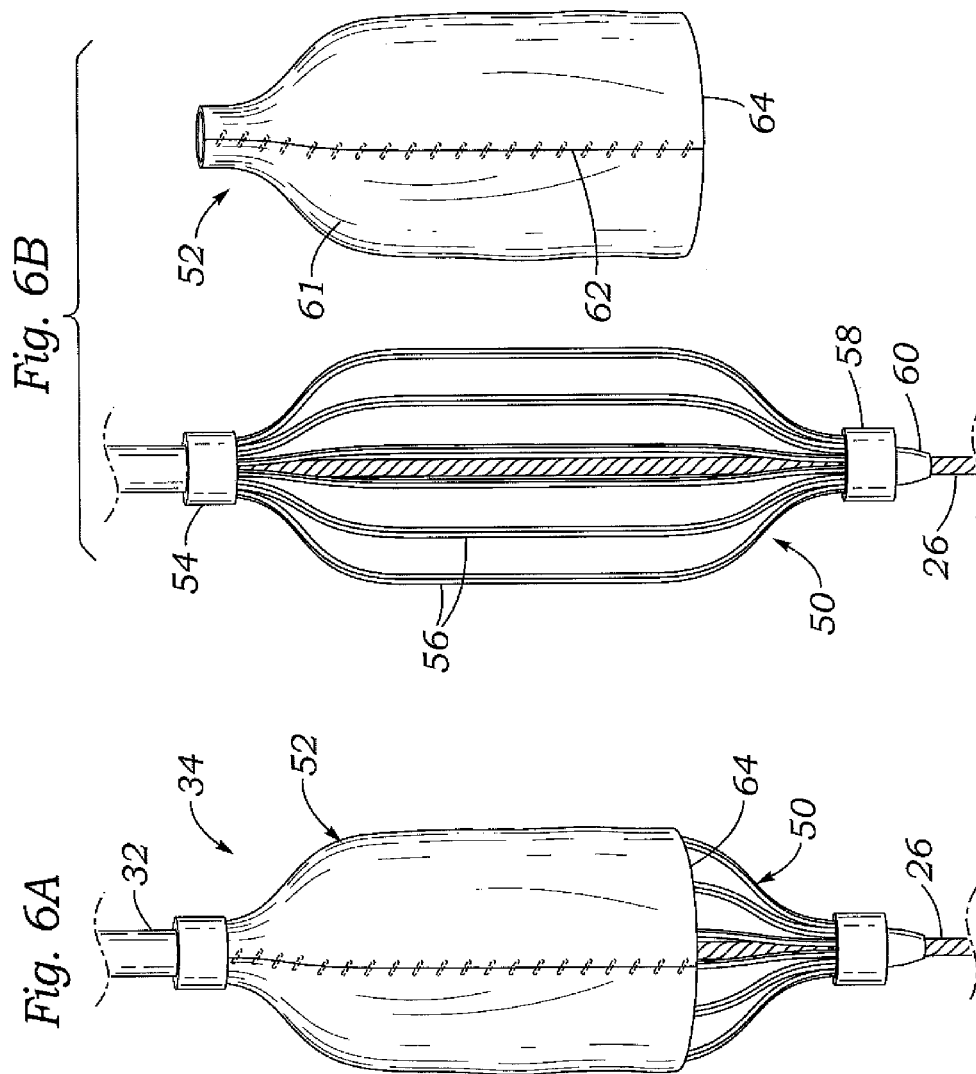
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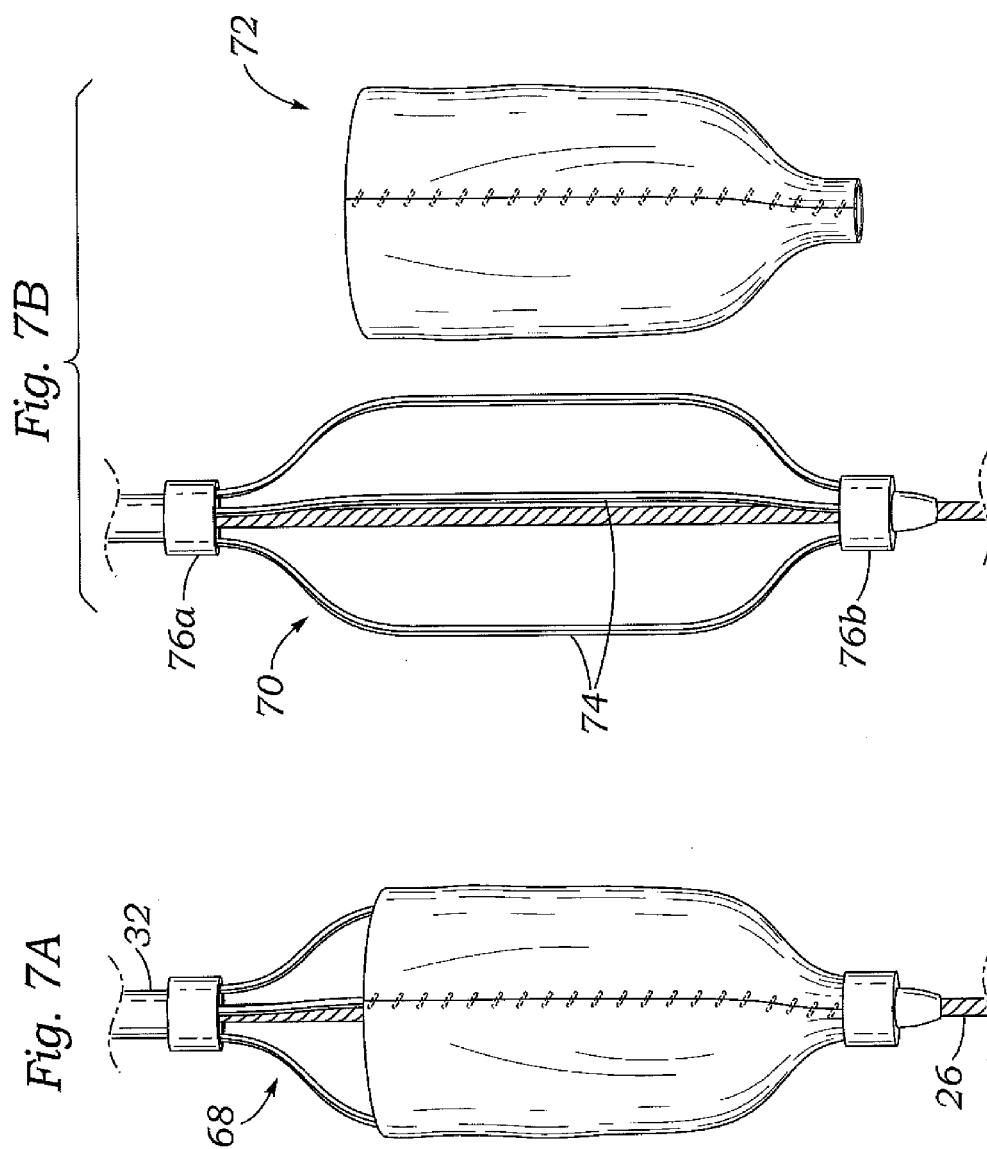


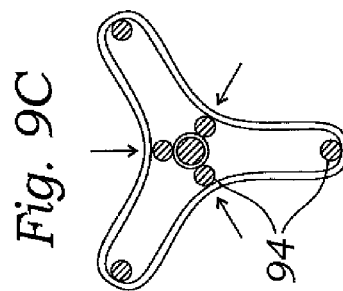
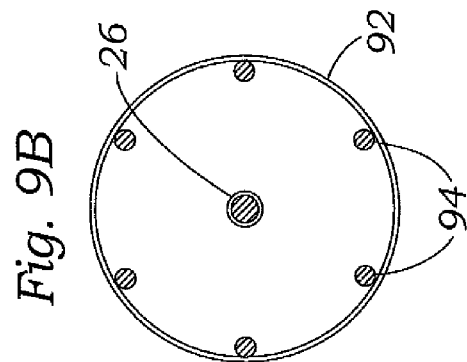
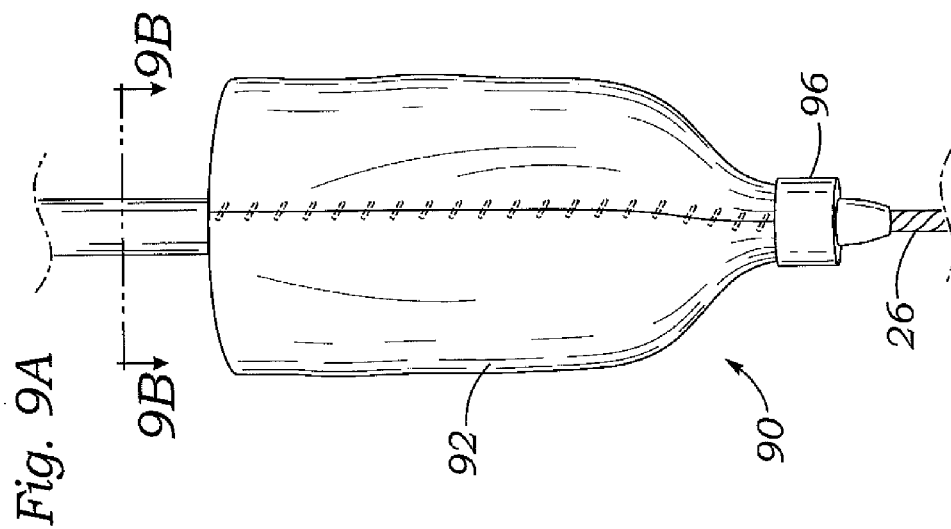
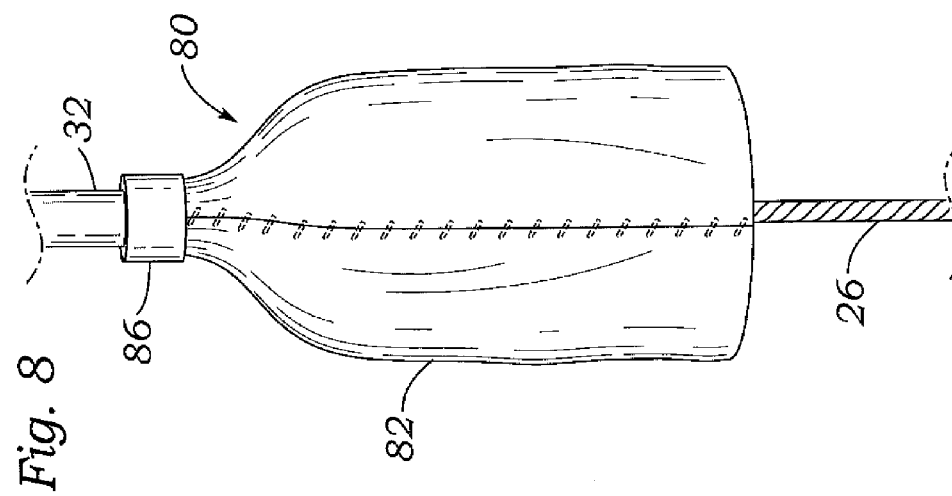


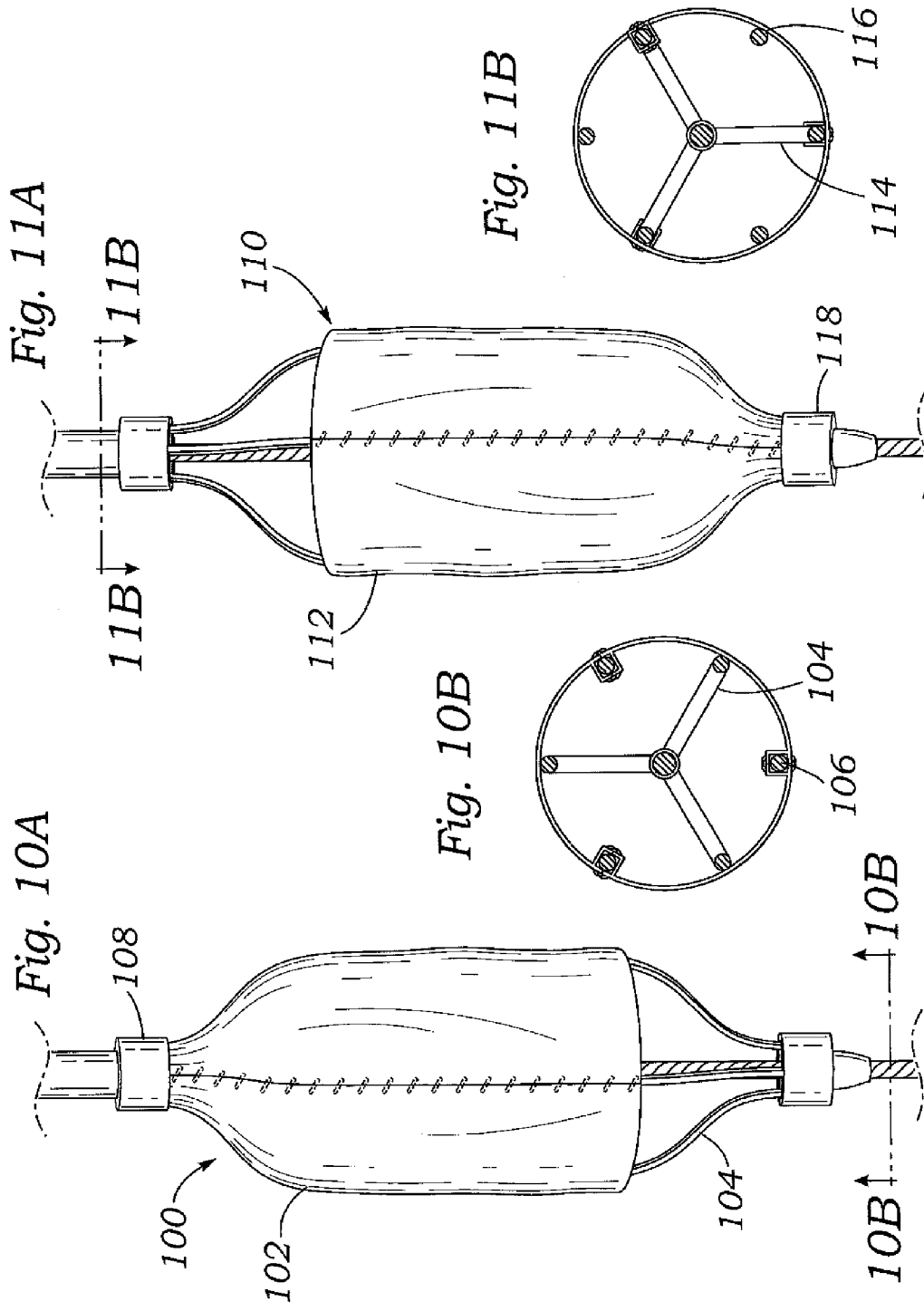


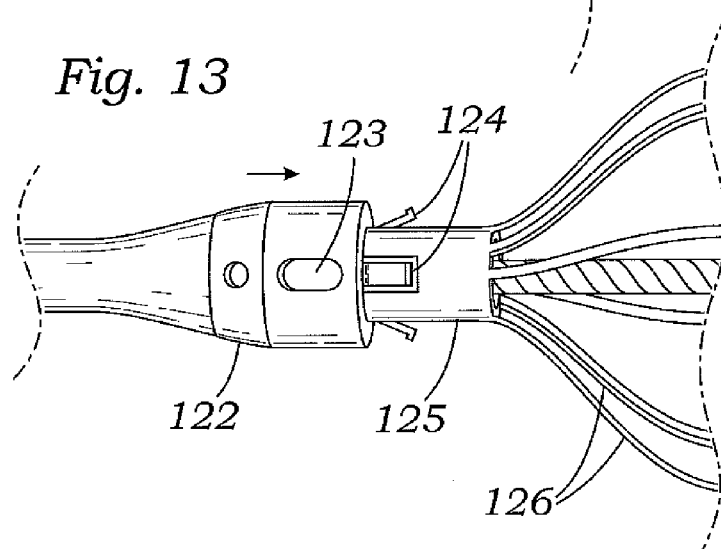
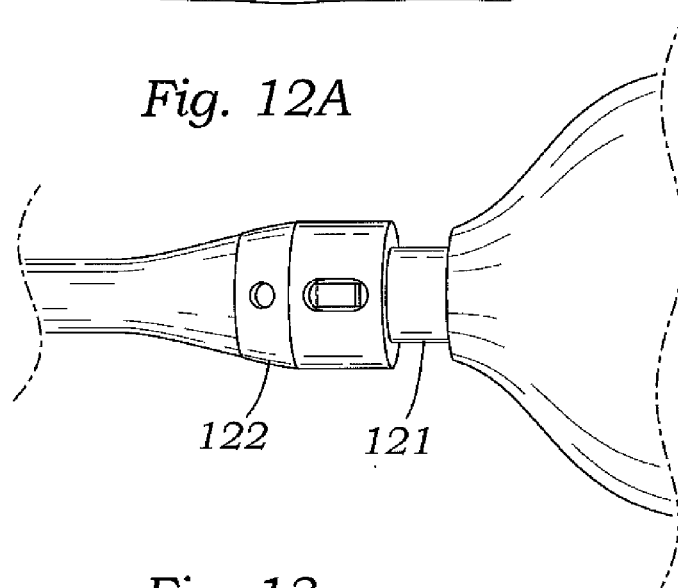
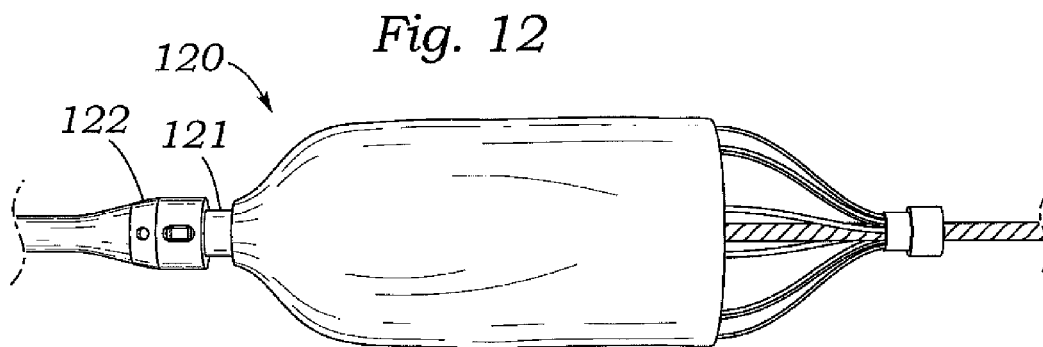












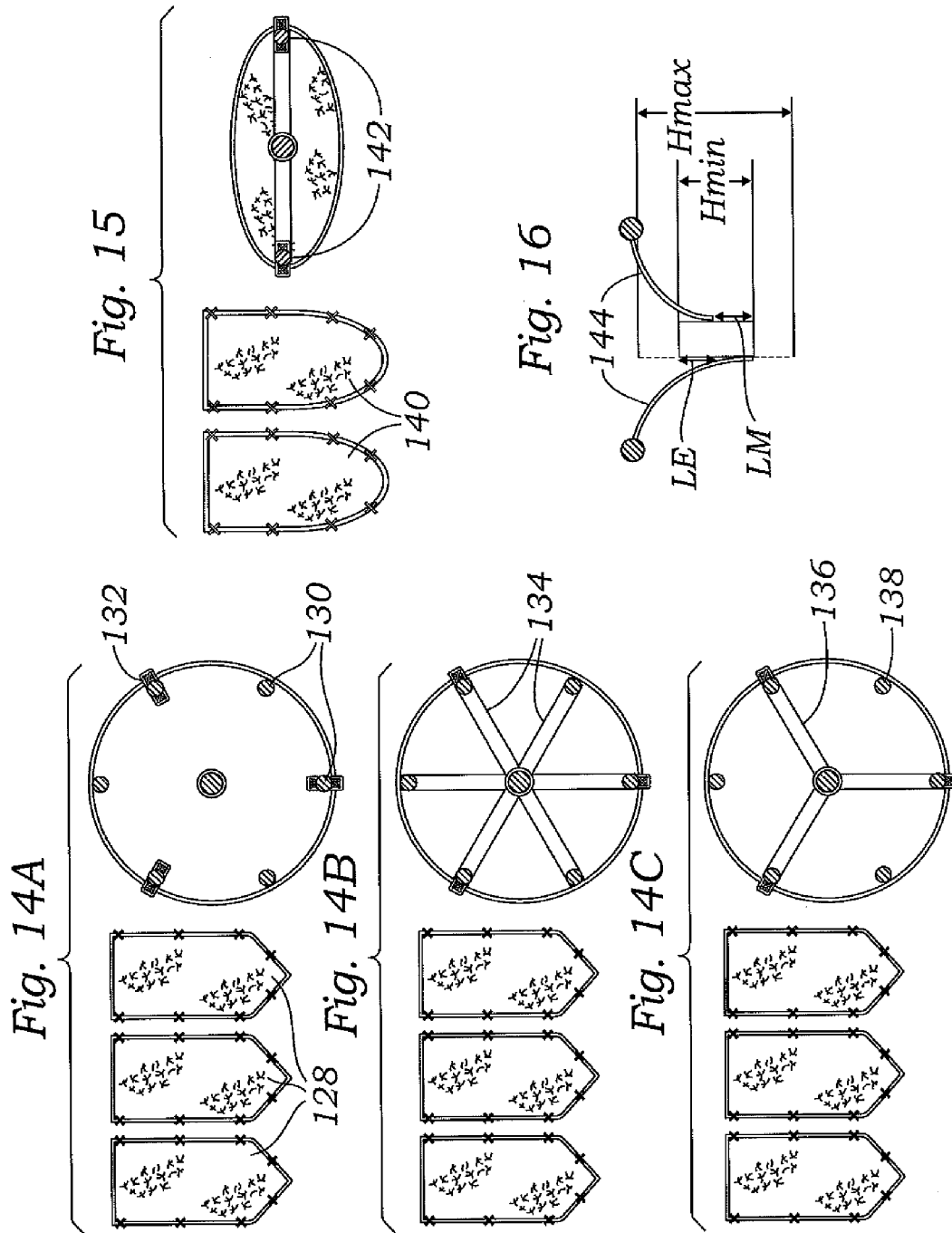


Fig. 17A

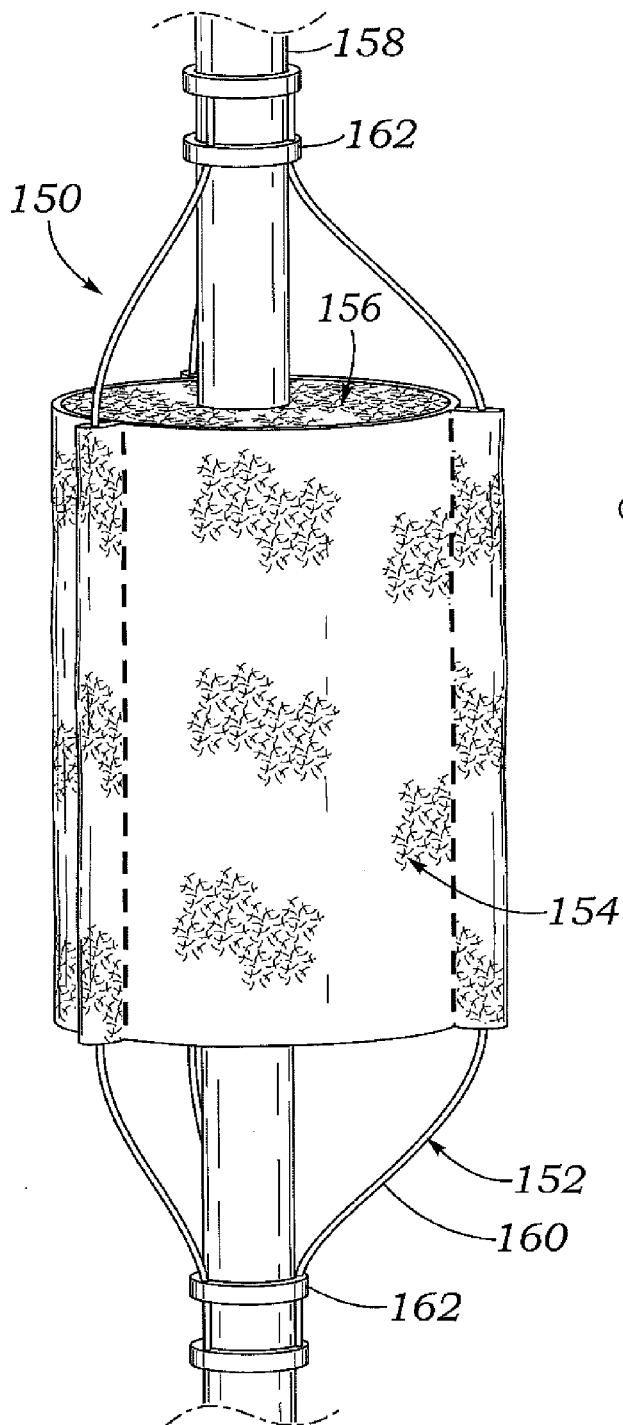


Fig. 17B

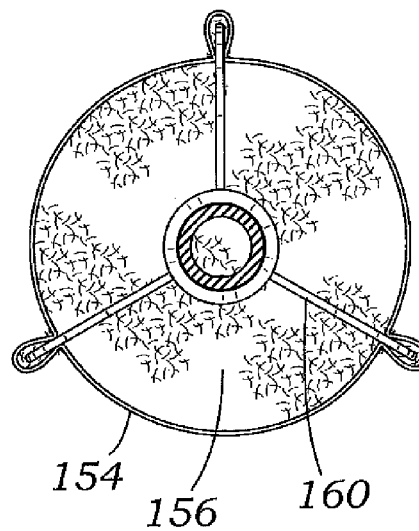
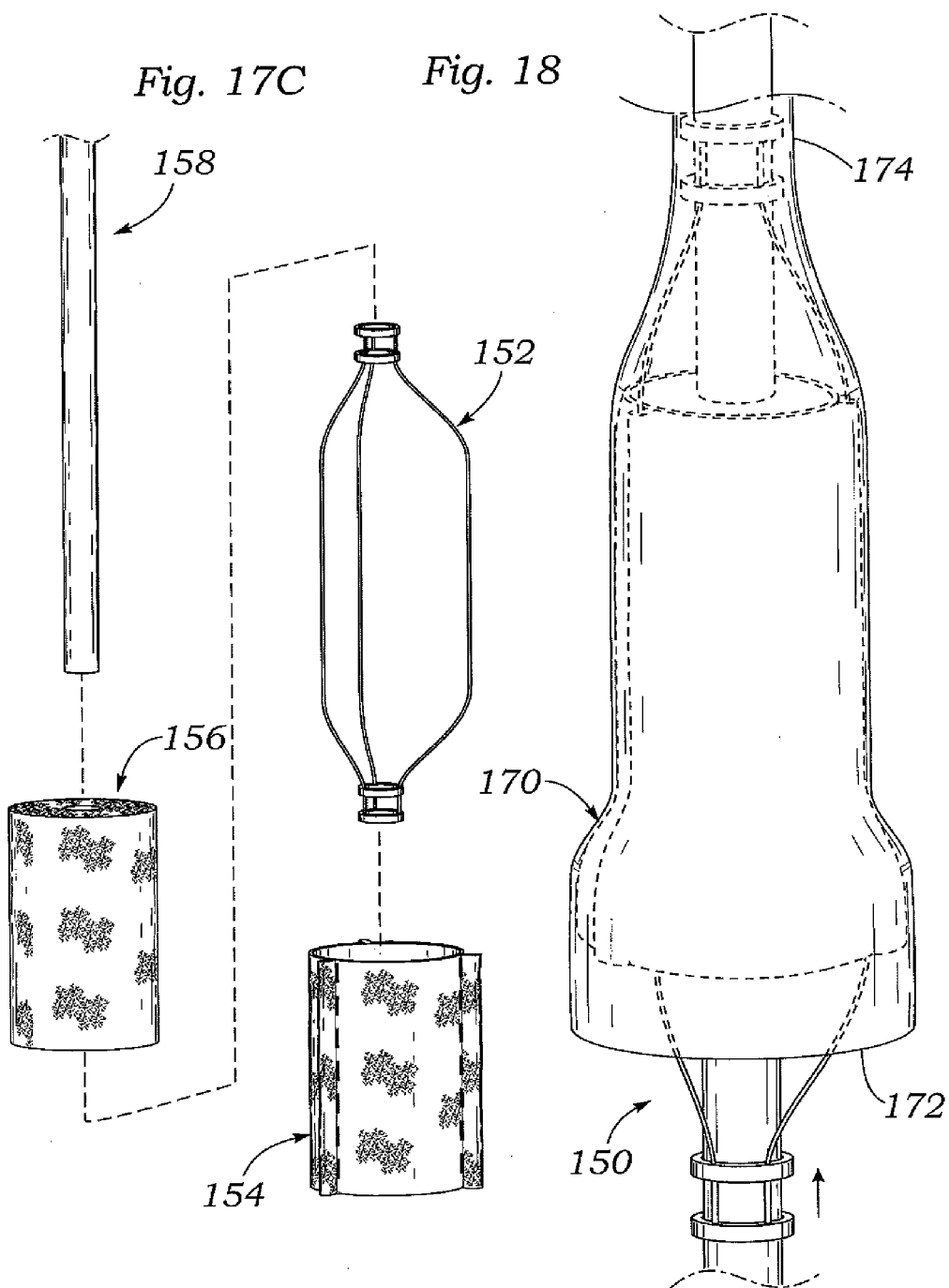
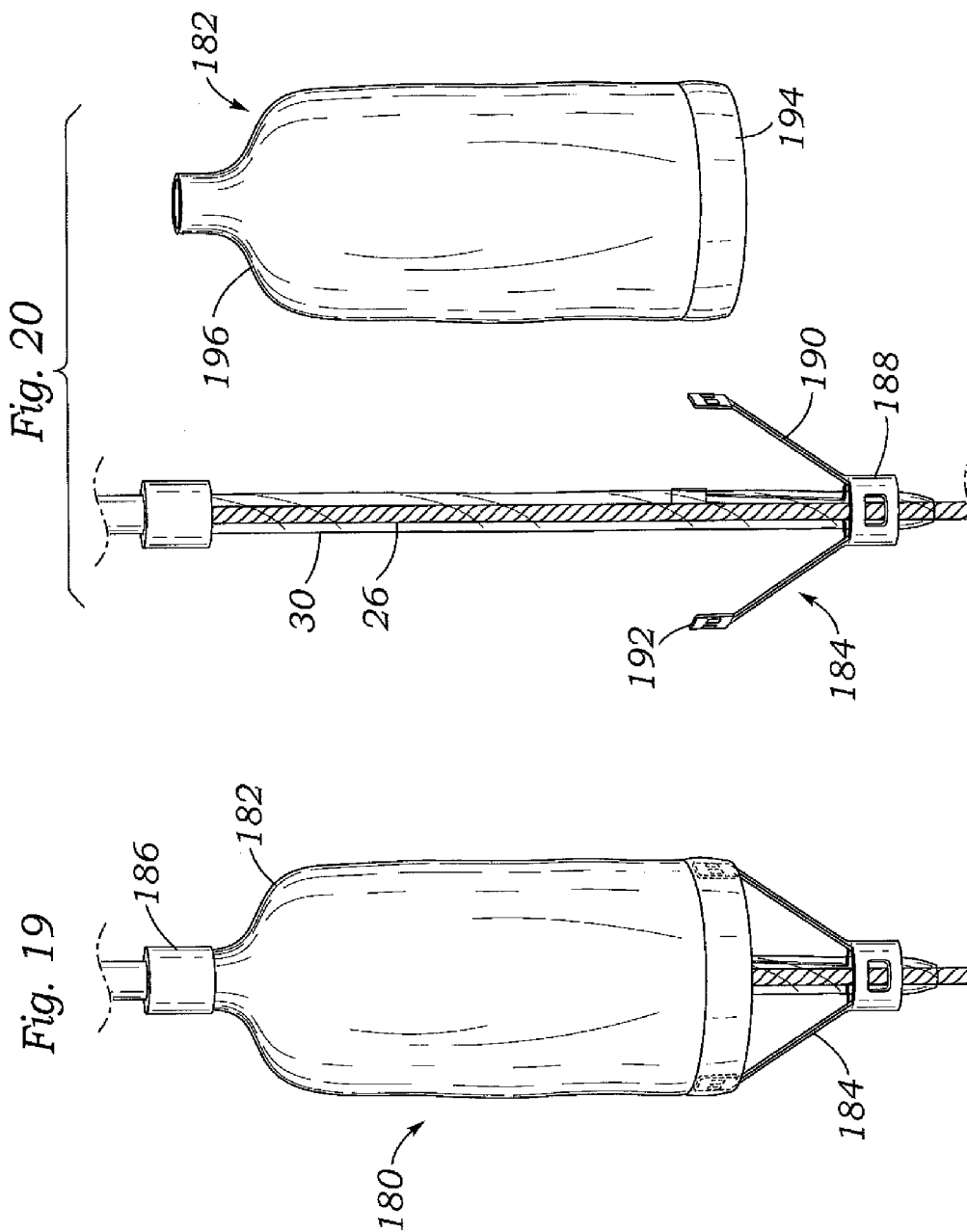


Fig. 17C

Fig. 18





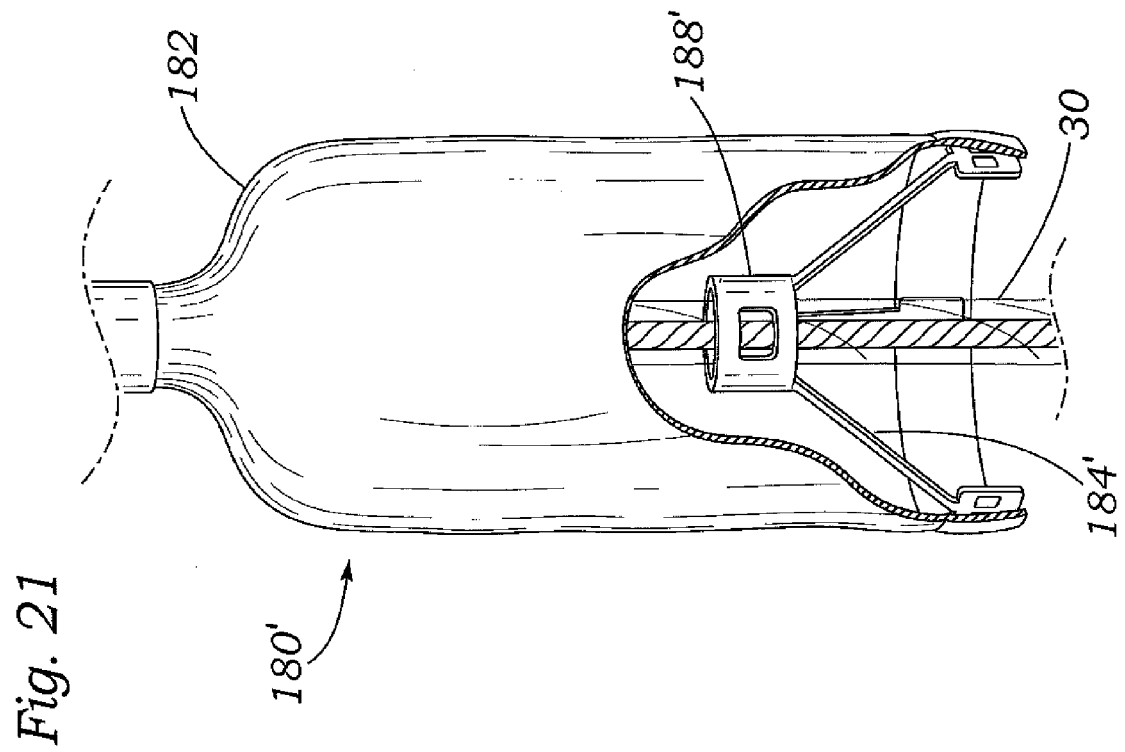


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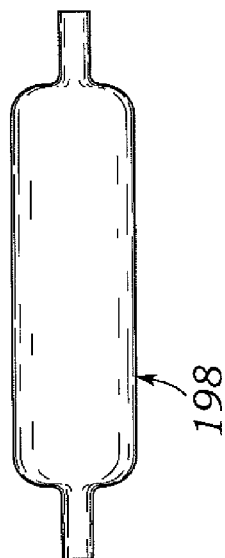


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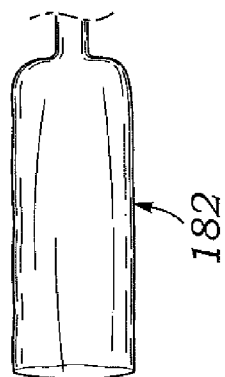


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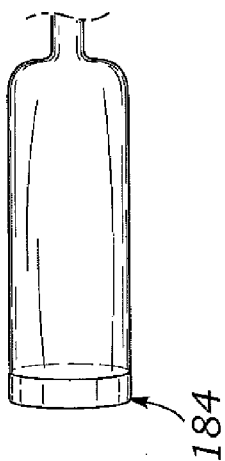


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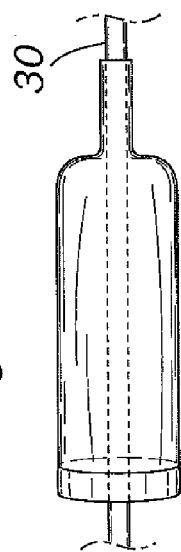


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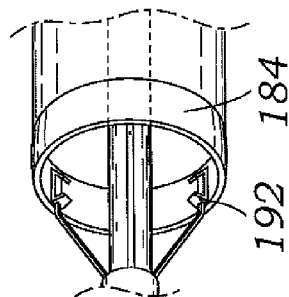


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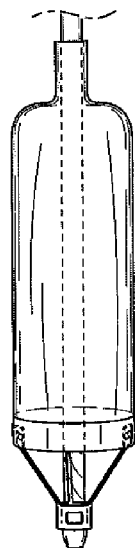
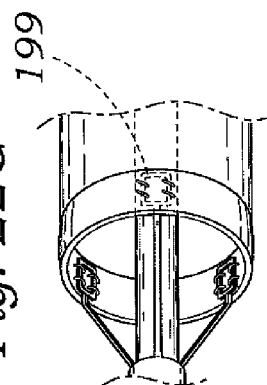
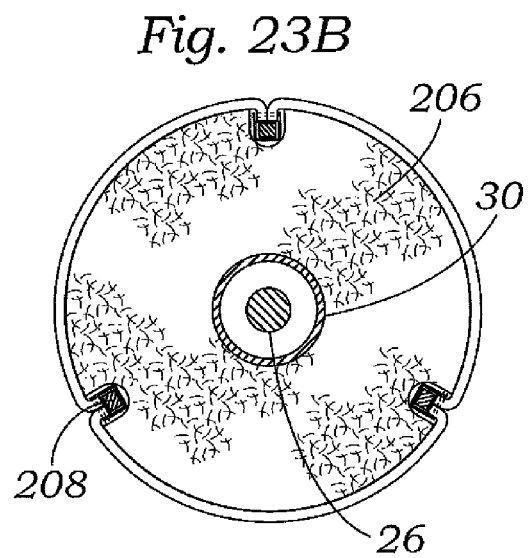
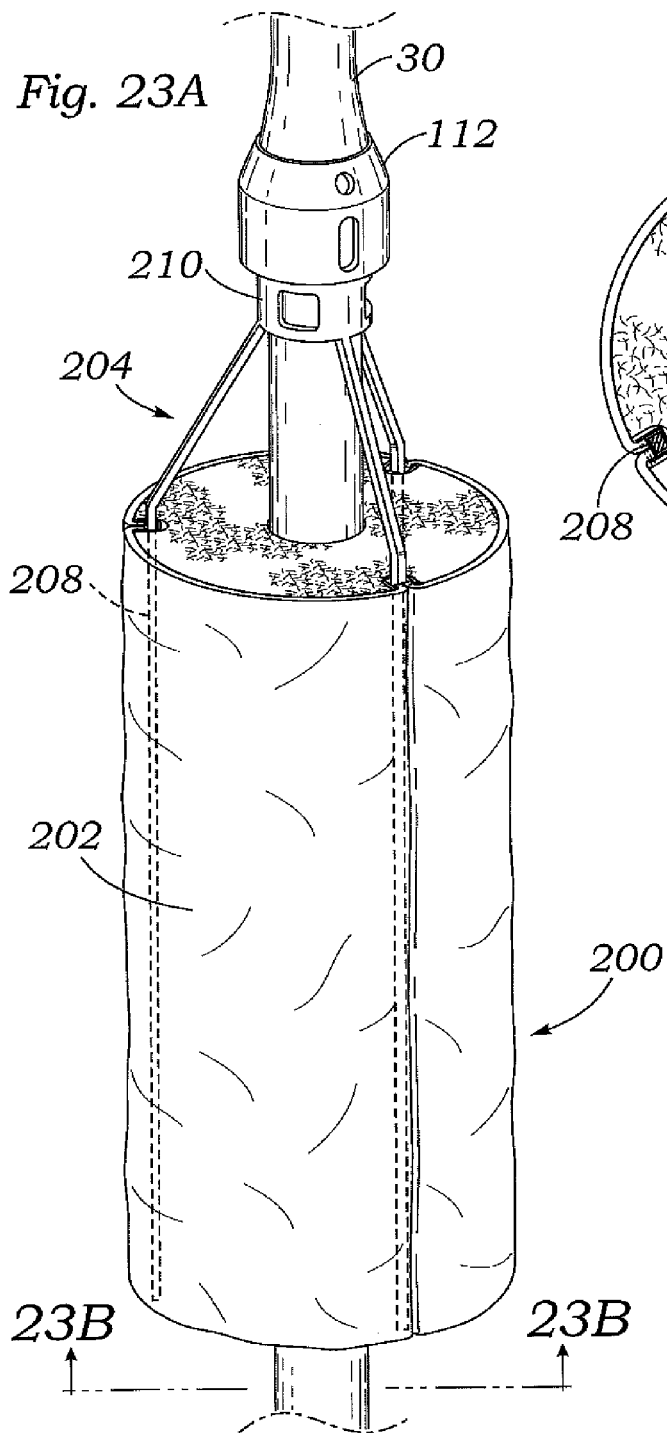
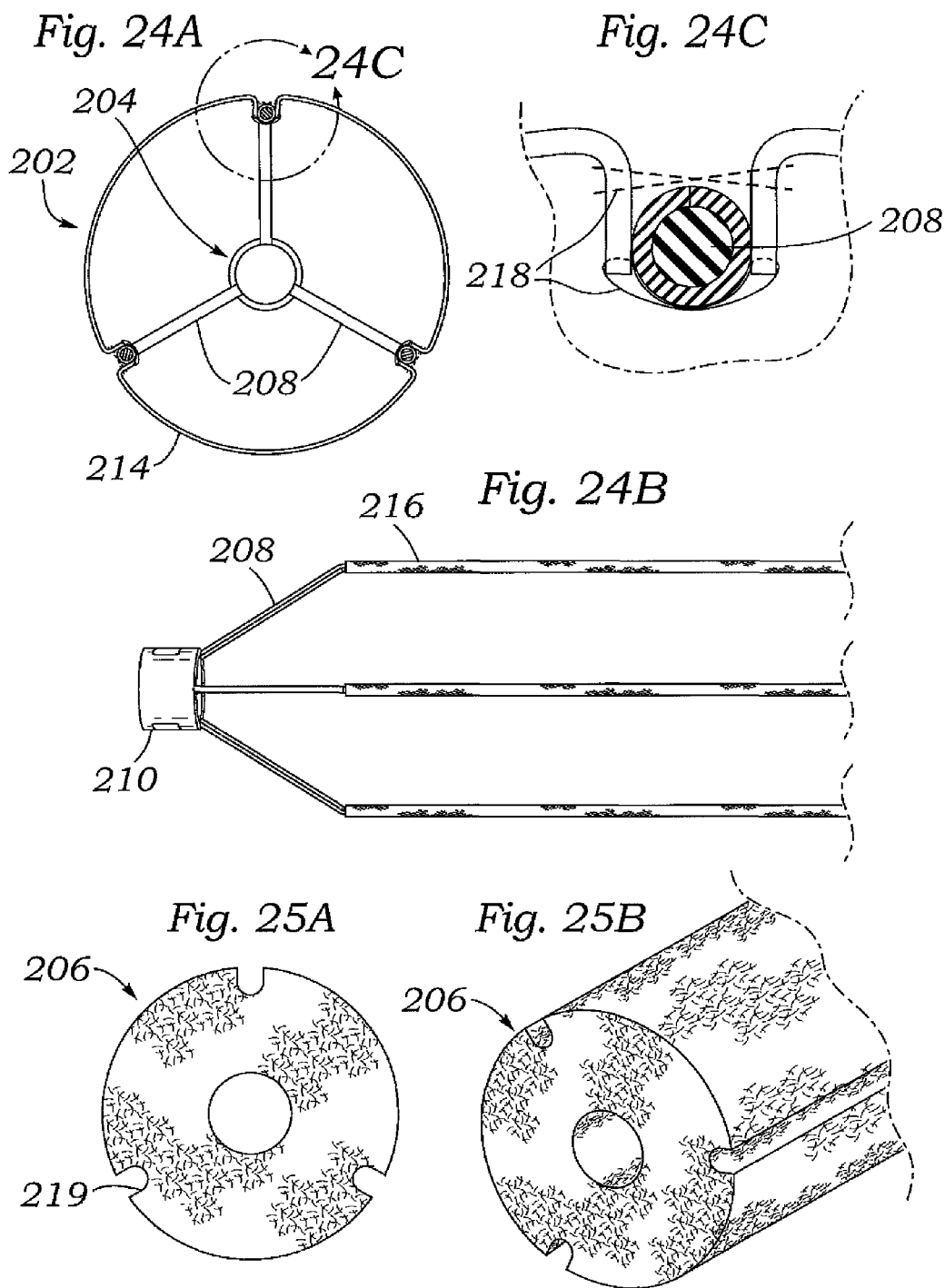


Fig. 22G







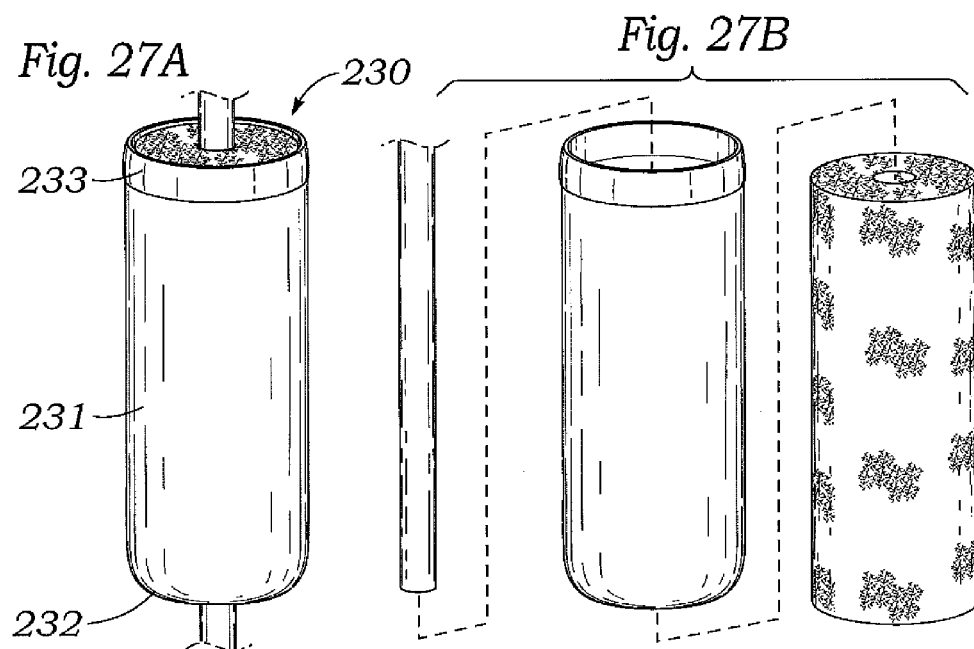
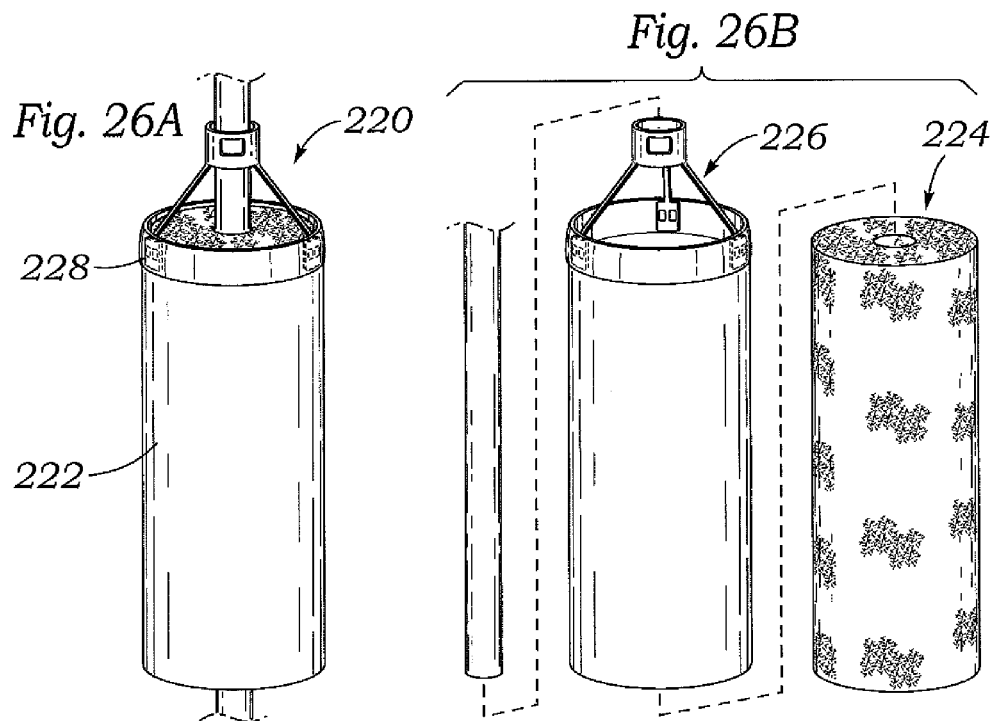


Fig. 28

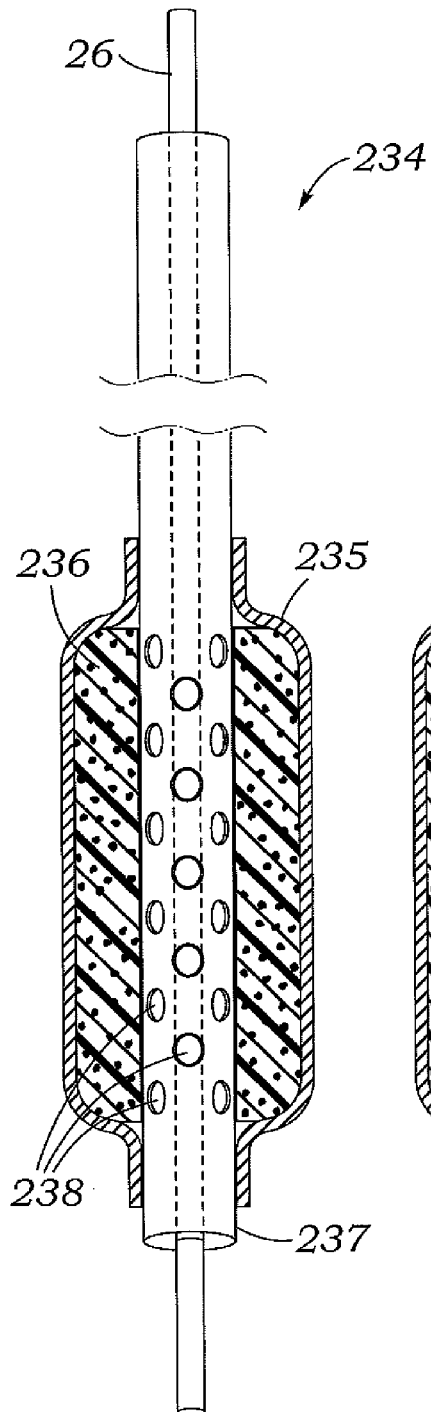


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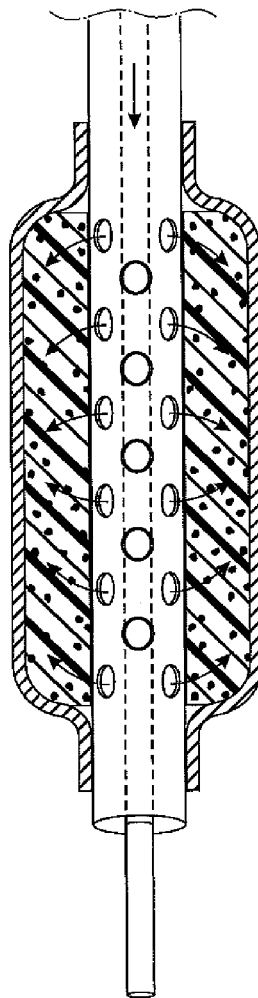
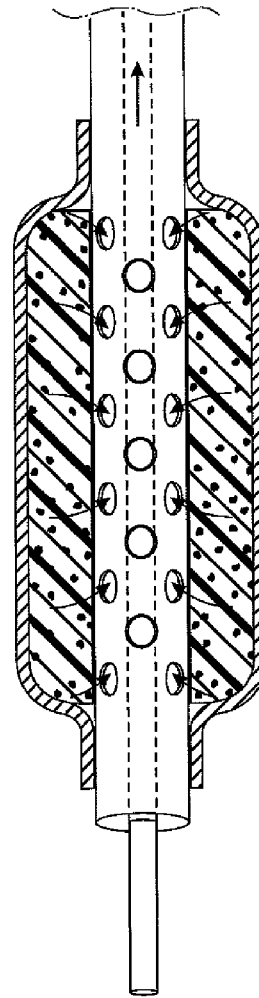


Fig. 29B



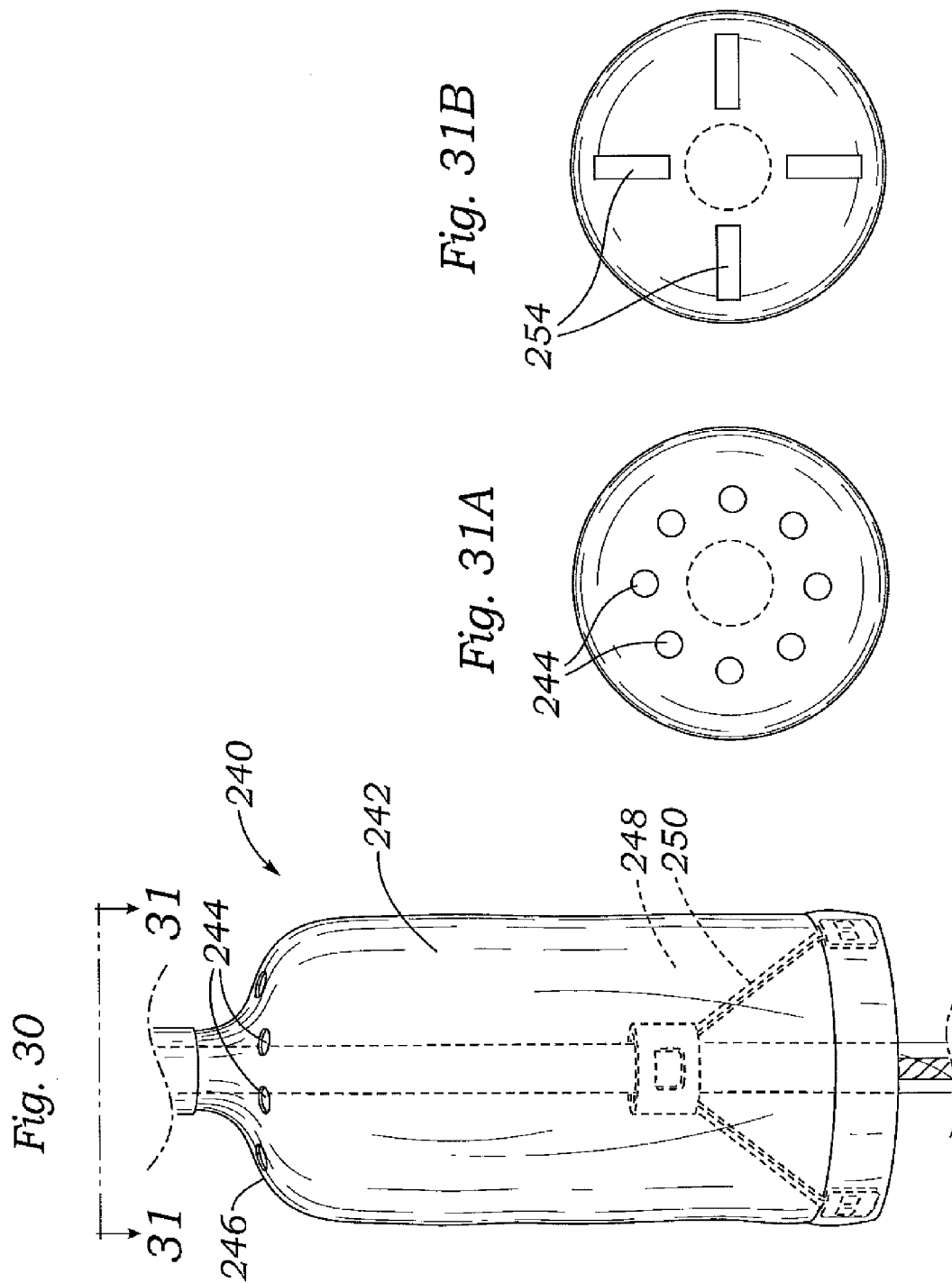


Fig. 32B

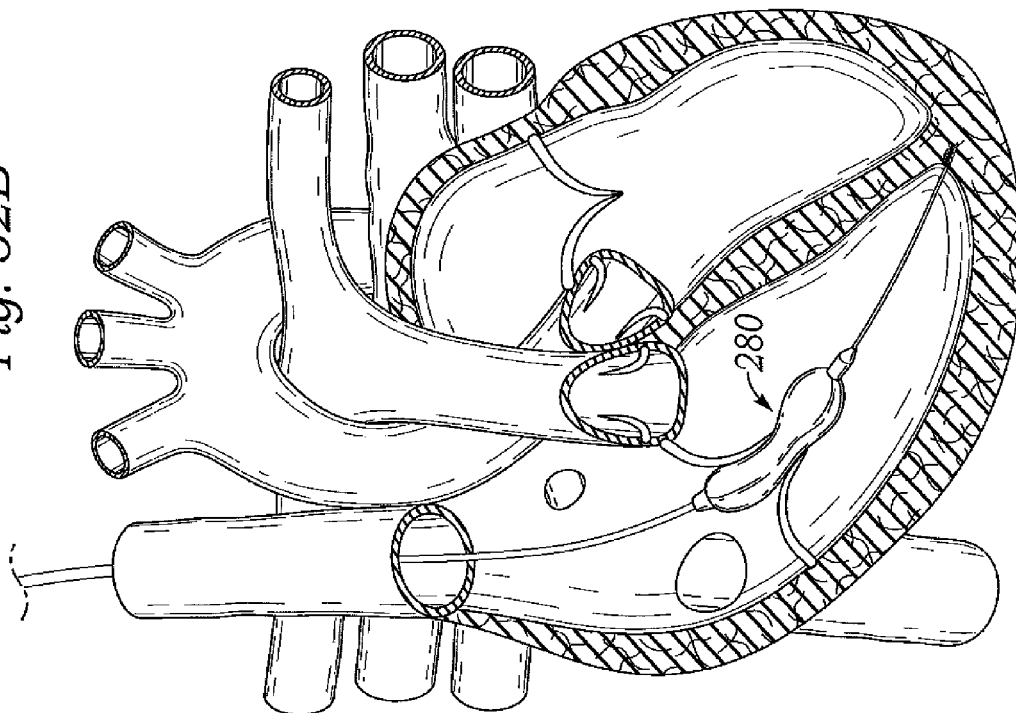
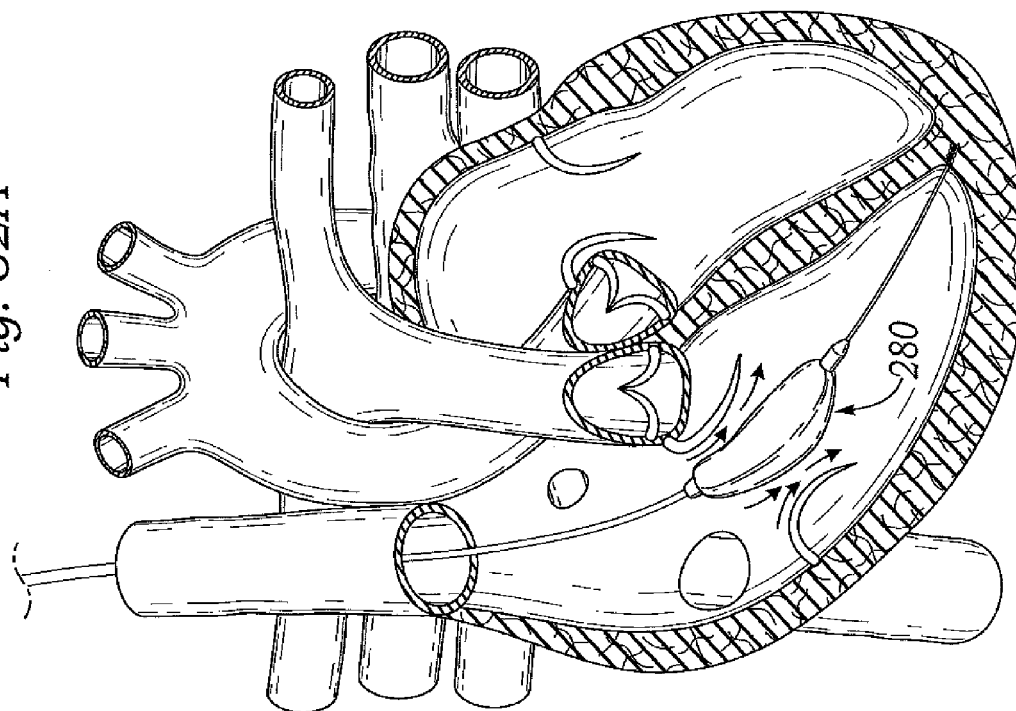


Fig. 32A



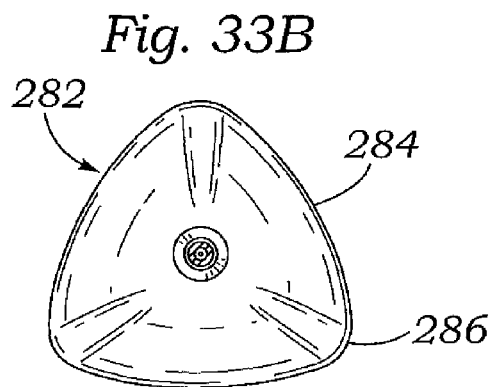
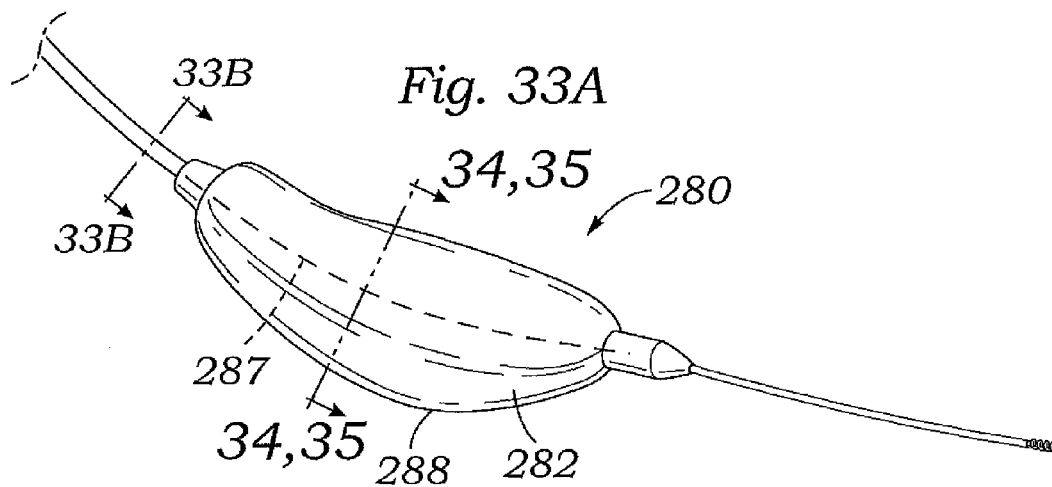


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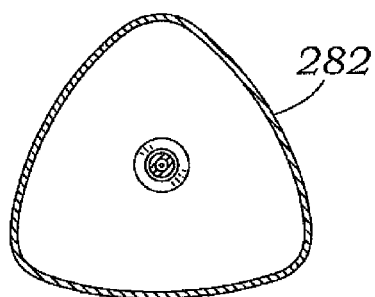


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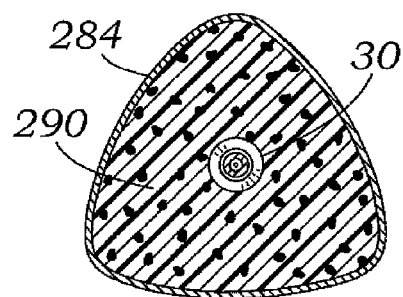


Fig. 36A

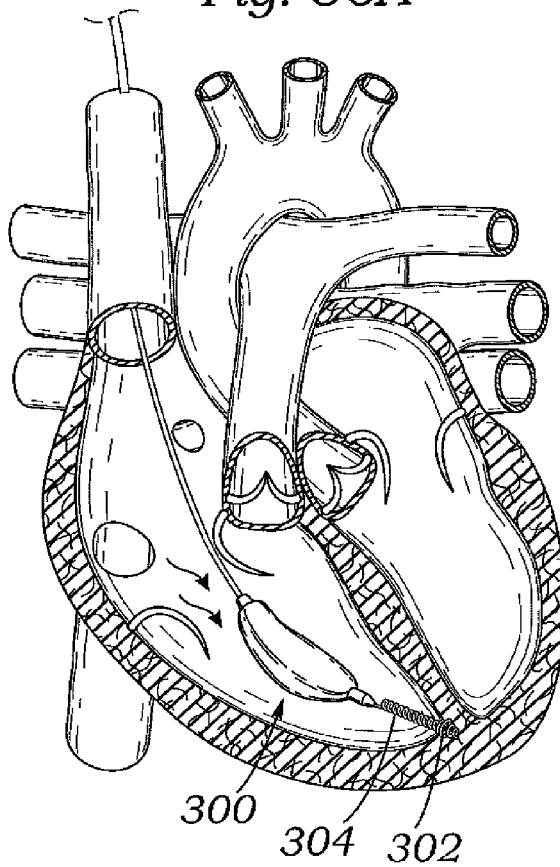


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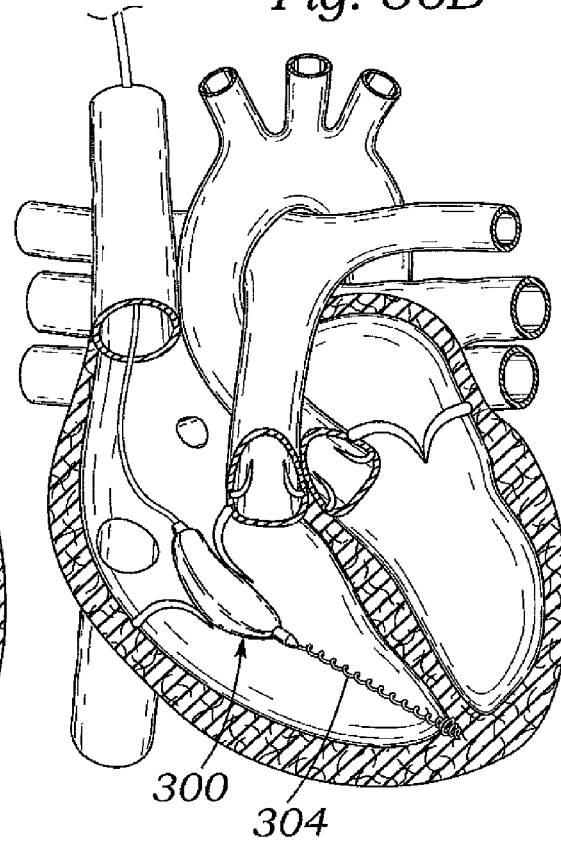


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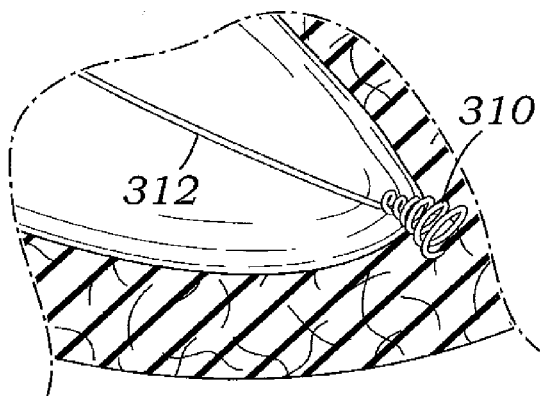


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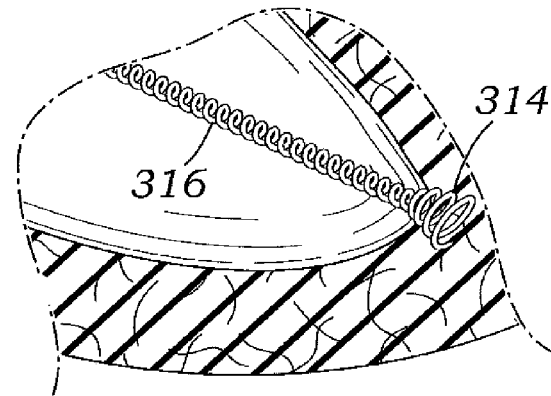


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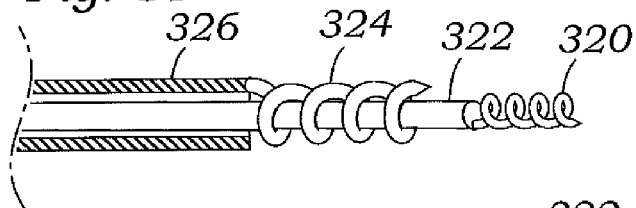


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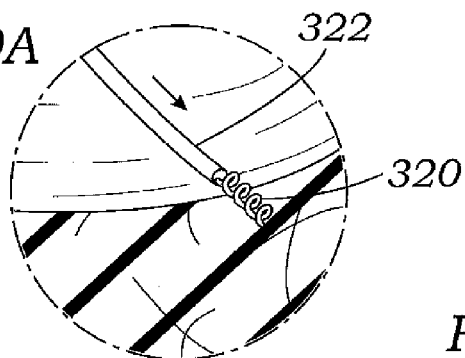


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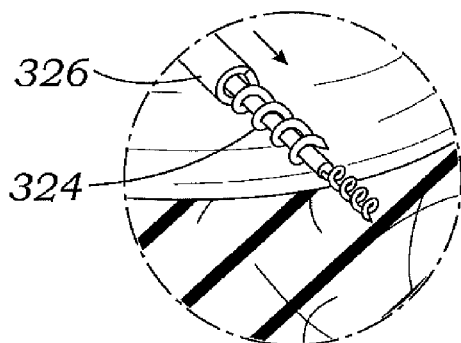


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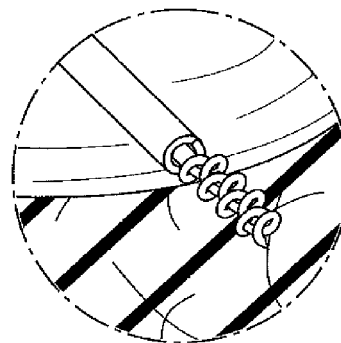


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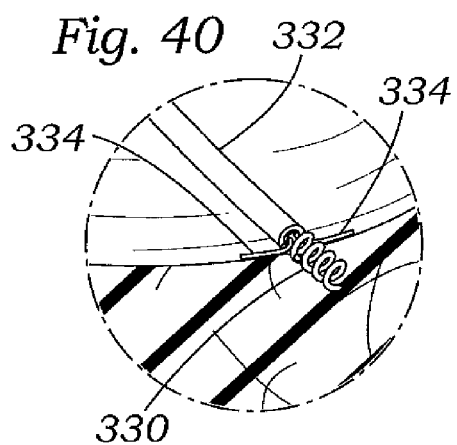


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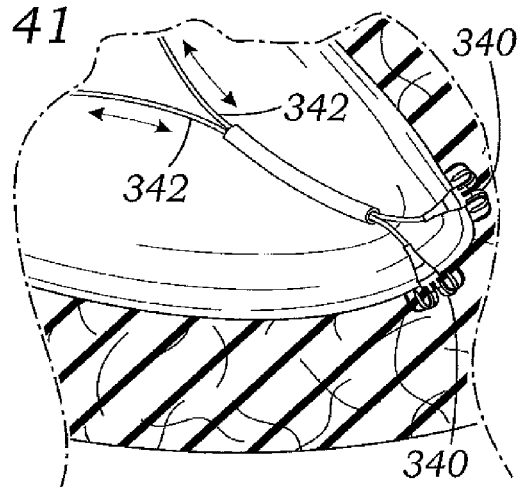


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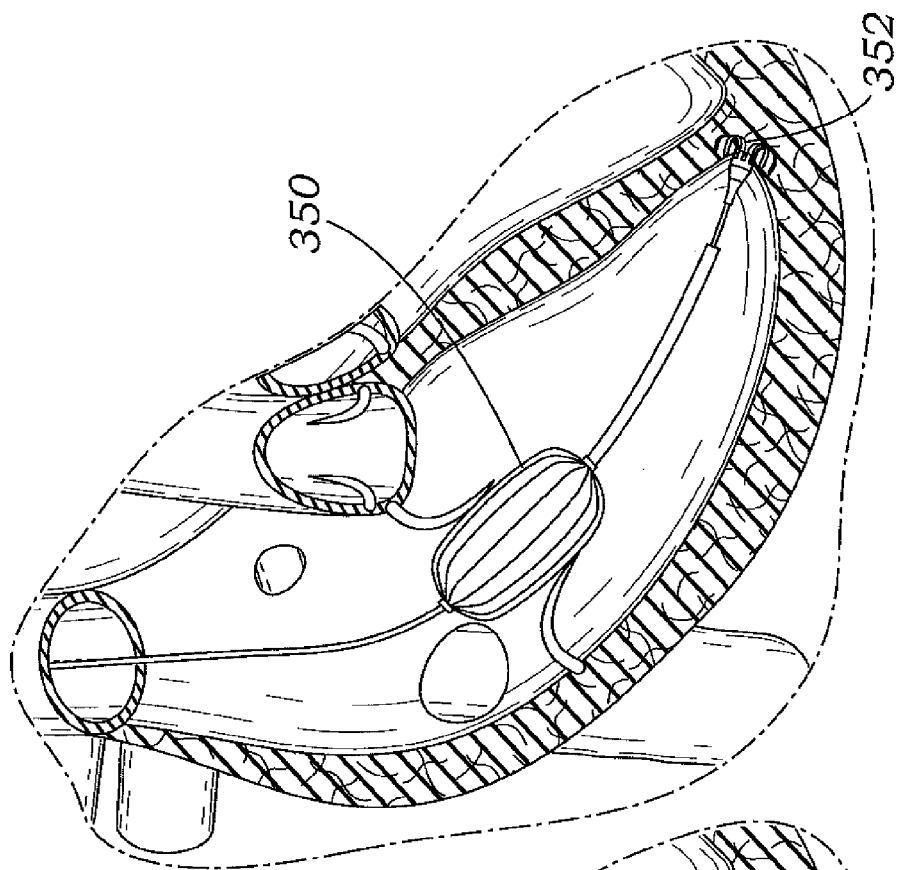


Fig. 42A

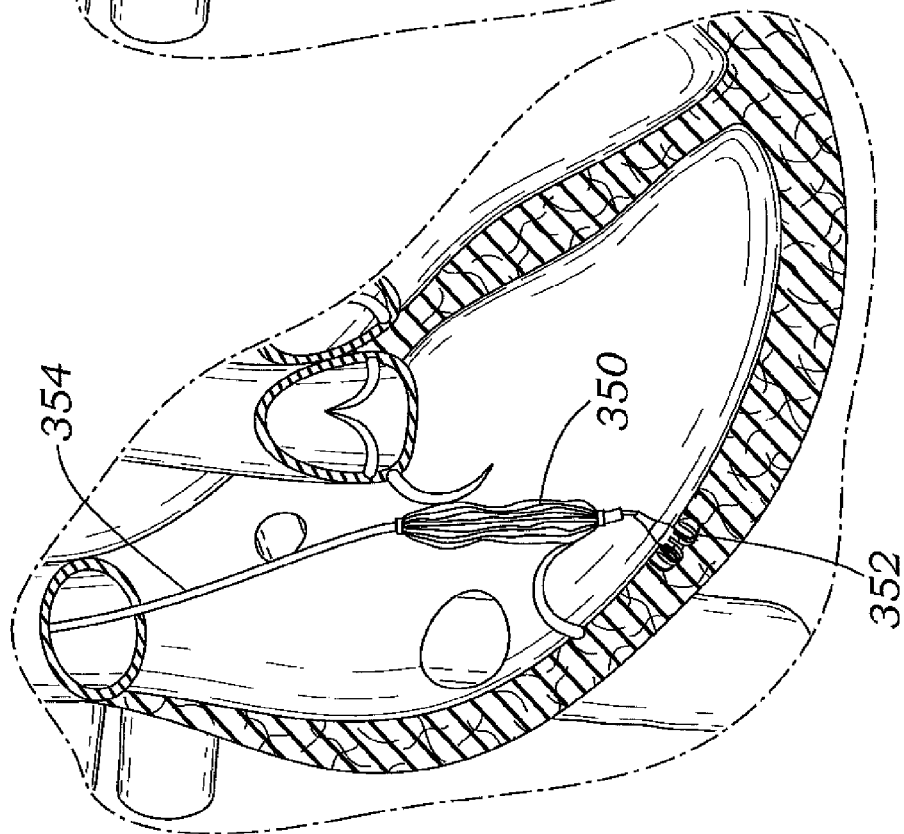


Fig. 43

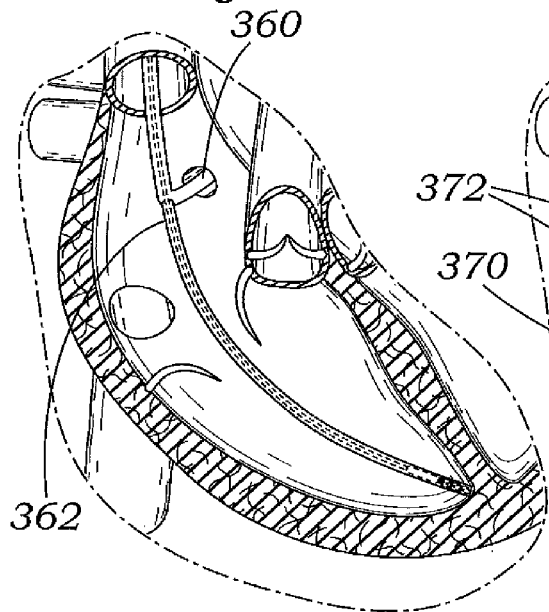


Fig. 44

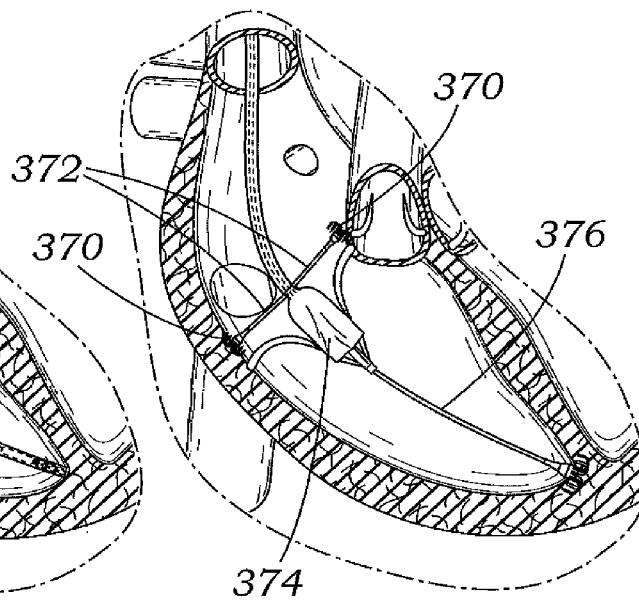
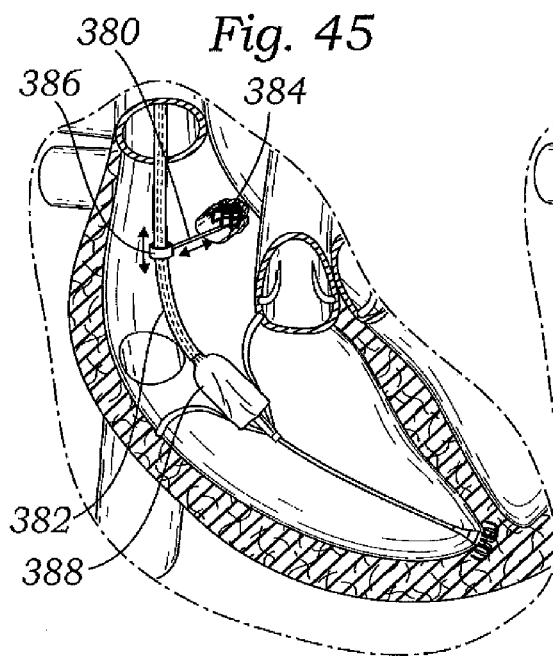
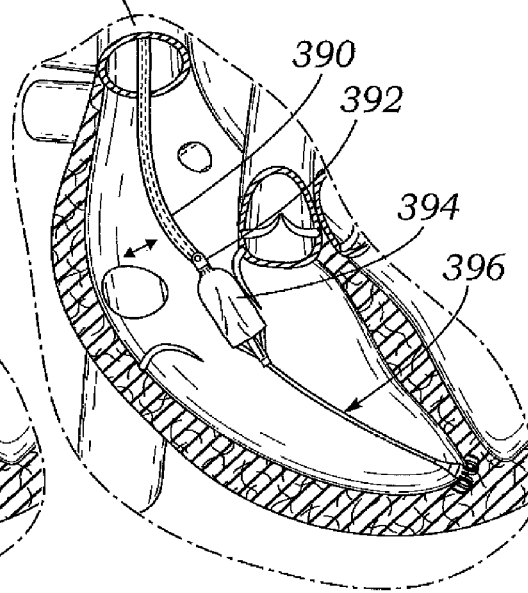


Fig. 45



SVC Fig. 46



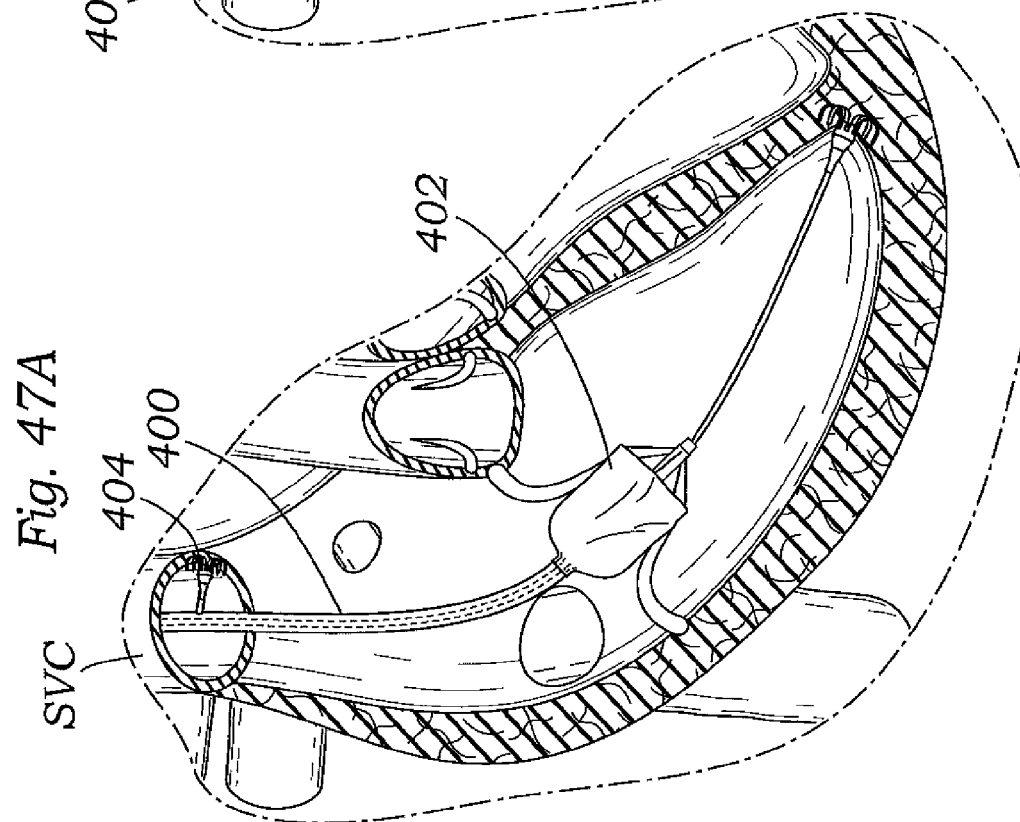
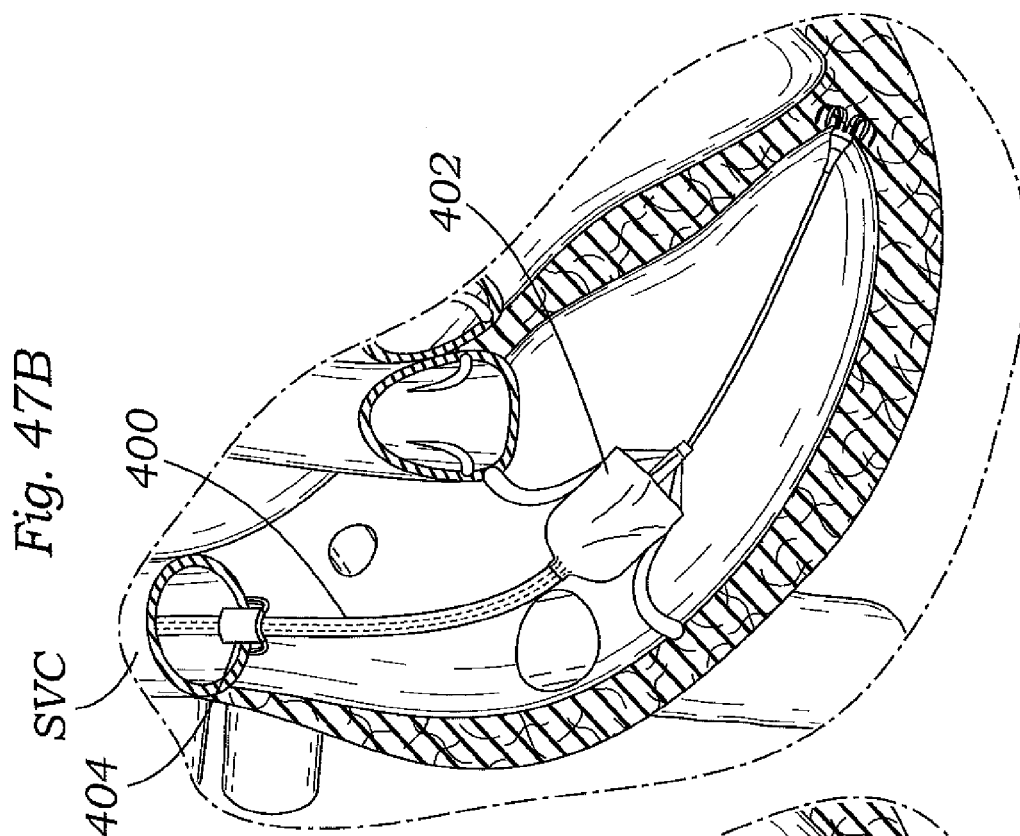


Fig. 48B

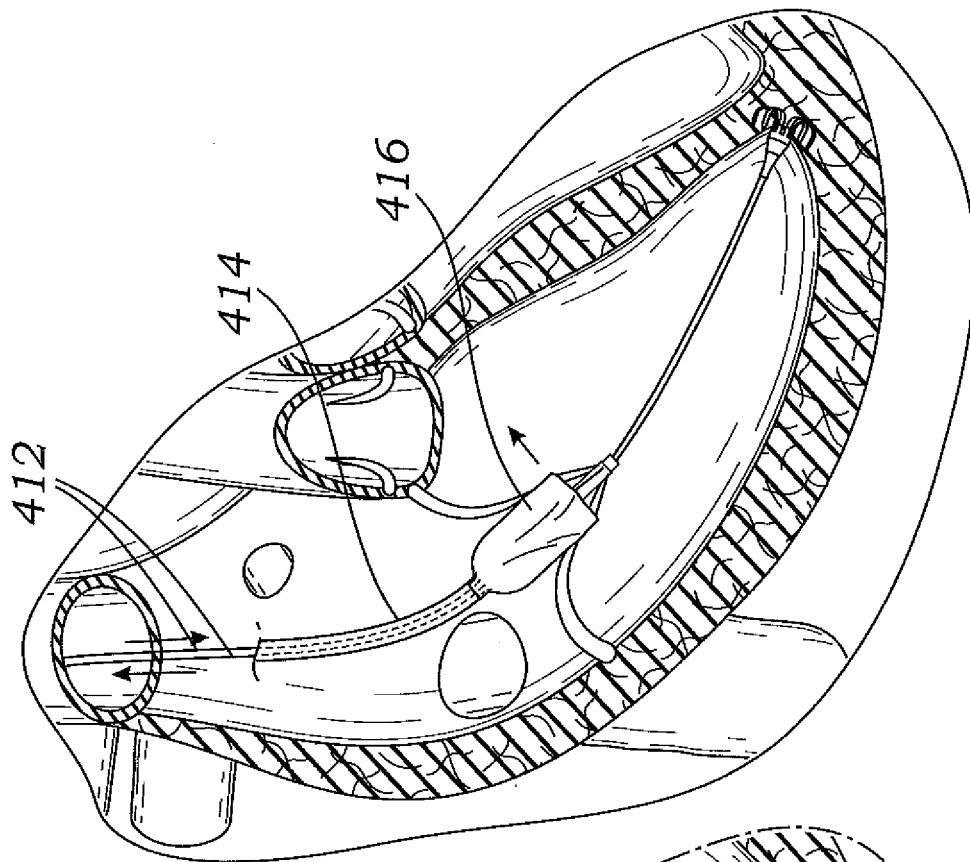
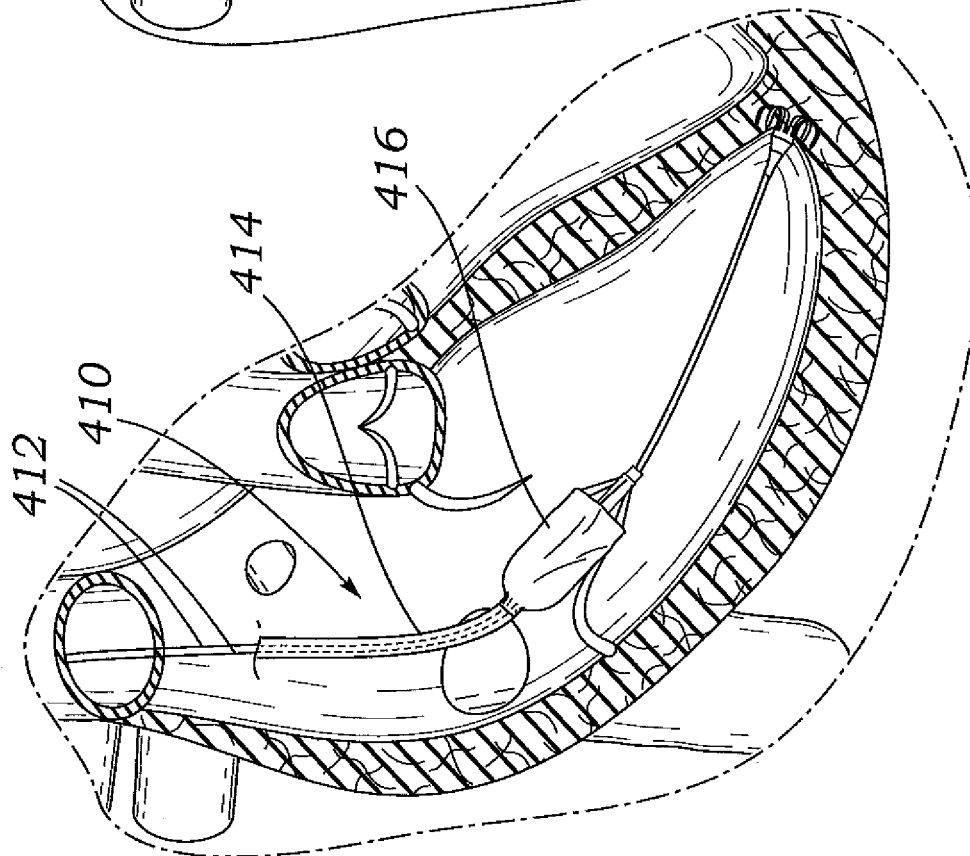
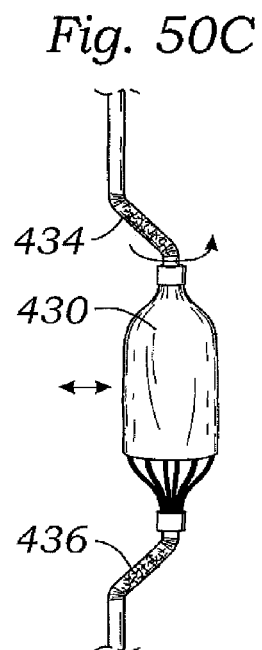
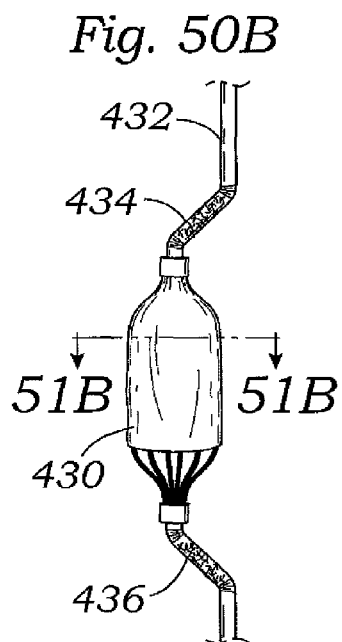
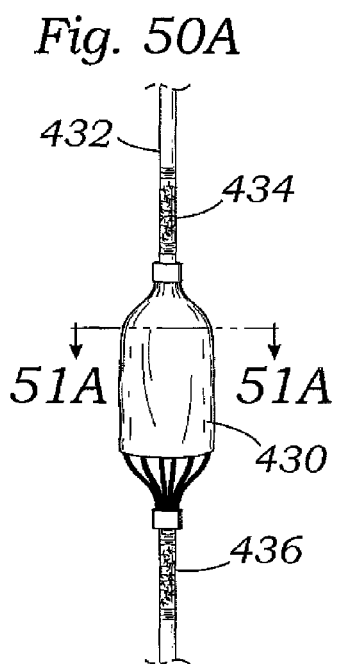
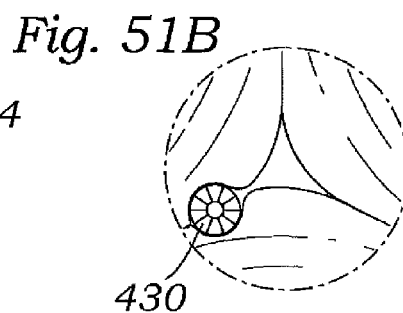
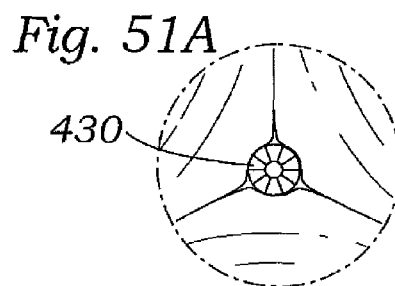
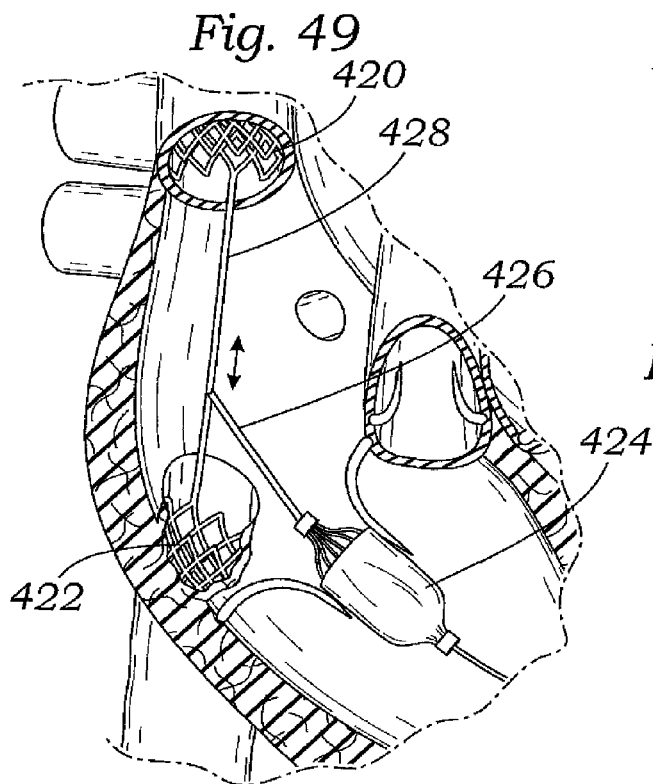


Fig. 48A





1

DEVICES AND METHODS FOR REDUCING CARDIAC VALVE REGURGITATION

RELATED APPLICATIONS

The present application claims priority under 35 U.S.C. §119 to U.S. Provisional Application Ser. No. 61/647,973, filed May 16, 2012, and to U.S. Provisional Application Ser. No. 61/734,728, filed Dec. 7, 2012, the disclosures of which are expressly incorporated herein by reference.

FIELD OF THE INVENTION

The present invention relates generally to devices and methods for improving the function of a defective heart valve. The devices and methods disclosed herein are particularly well adapted for implantation in a patient's heart for reducing regurgitation through a heart valve.

BACKGROUND OF THE INVENTION

The function of the heart may be seriously impaired if any of the heart valves are not functioning properly. The heart valves may lose their ability to close properly due to e.g. dilation of an annulus around the valve, ventricular dilation, or a leaflet being flaccid causing a prolapsing leaflet. The leaflets may also have shrunk due to disease, e.g. rheumatic disease, and thereby leave a gap in the valve between the leaflets. The inability of the heart valve to close properly can cause a leak backwards (i.e., from the outflow to the inflow side), commonly referred to as regurgitation, through the valve. Heart valve regurgitation may seriously impair the function of the heart since more blood will have to be pumped through the regurgitating valve to maintain adequate circulation. Heart valve regurgitation decreases the efficiency of the heart, reduces blood circulation, and adds stress to the heart. In early stages, heart valve regurgitation leaves a person fatigued or short of breath. If left unchecked, the problem can lead to congestive heart failure, arrhythmias or death.

Heart valve disease, such as valve regurgitation, is typically treated by replacing or repairing the diseased valve during open-heart surgery. However, open-heart surgery is highly invasive and is therefore not an option for many patients. For high-risk patients, a less-invasive method for repair of heart valves is considered generally advantageous.

Accordingly, there is an urgent need for an alternative device and method of use for treating heart valve disease in a minimally invasive procedure that does not require extracorporeal circulation. It is especially desirable that embodiments of such a device and method be capable of reducing or eliminating regurgitation through a tricuspid heart valve. It is also desirable that embodiments of such a device and method be well-suited for treating a mitral valve. It is also desirable that such a device be safe, reliable and easy to deliver. It is also desirable that embodiments of such a device and method be applicable for improving heart valve function for a wide variety of heart valve defects. It is also desirable that embodiments of such a device and method be capable of improving valve function without replacing the native valve. The present invention addresses this need.

SUMMARY OF THE INVENTION

The present invention relates generally to devices and methods for improving the function of a defective heart valve. The devices and methods disclosed herein are par-

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ticularly well adapted for implantation in a patient's heart for reducing regurgitation through a heart valve. The devices and methods disclosed herein are particularly useful in reducing regurgitation through the two atrioventricular (AV) valves, which are between the atria and the ventricles—i.e., the mitral valve and the tricuspid valve.

In one embodiment, the device comprises: an anchor to deploy in the tissue of the right ventricle, a flexible anchor rail connected to the anchor, a coaptation element that rides over the anchor rail, a catheter attached to the proximal end of the coaptation element, a locking mechanism to fix the position of the coaptation element relative to the anchor rail, and a proximal anchoring feature to fix the proximal end of the coaptation catheter subcutaneously in the subclavian vein.

In another particular embodiment, the coaptation element consists of a hybrid structure: a series of a plurality (preferably three or more) flexible metallic struts to define a mechanical frame structure or a compressible biocompatible material, and a covering of pericardium or some other biocompatible material to provide a coaptation surface around which the native leaflets can form a seal. The flexible struts desirably attach to a catheter shaft on their proximal and/or distal ends, and collapse into a smaller diameter in order to be delivered through a low profile sheath. In particular, the struts attach on one end or both to a catheter shaft, and are complete or interrupted, they typically extend the length of the element, extend out or inwards, and may be discrete struts or a more connected mesh. The mechanical frame typically expands to the larger shape passively upon exiting a protective sheath via shape memory properties (e.g. Nitinol), but could also be expanded via longitudinal compression of the catheter, a shape memory balloon or some other external force. Additionally, the coaptation element can be an open or closed structure, any biocompatible material and framework that allows for compressibility for delivery and expands either actively or passively upon delivery, can be various shapes, and can be a passive or active element that is responsive to the cardiac cycle to change shapes to accommodate the regurgitant orifice.

In accordance with a preferred embodiment, a heart valve coaptation system for reducing regurgitation through the valve comprises a flexible rail having a ventricular anchor on the distal end thereof adapted to anchor into tissue within a ventricle. A delivery catheter has a lumen through which the flexible rail passes, and a coaptation member fixed on a distal end of the delivery catheter has a bell-shaped cover with a first end open and a flexible inner support holding the first end open. Finally, a locking collet on the delivery catheter secures the axial position of the coaptation member and delivery catheter on the flexible rail.

The locking collet preferably includes a pair of internally threaded tubular grips each fixed to one of two separate sections of the delivery catheter and engaging a common externally threaded tubular shaft member. The tubular grips act on a wedge member interposed between at least one of the grips and the flexible rail to securing the axial position of the coaptation member and delivery catheter on the flexible rail. The first end of the bell-shaped cover of the coaptation member may be on a distal or ventricular side thereof, or on the proximal or atrial side. The second end of the bell-shaped cover may have flow through openings to help avoid blood stagnation. The flexible inner support may comprise a flexible frame with struts emanating from a central collar and engaging the first end of the bell-shaped cover, or with struts that extend substantially the length of the bell-shaped cover. Alternatively, the flexible inner sup-

port comprises a compressible foam member substantially filling the cover. The cover may be formed of polycarbonate urethane, or may be bioprosthetic tissue.

Another exemplary embodiment of a heart valve coaptation system for reducing regurgitation through the valve again includes a flexible rail having a ventricular anchor on the distal end thereof adapted to anchor into tissue within a ventricle, and a delivery catheter having a lumen through which the flexible rail passes. A coaptation member fixed on a distal end of the delivery catheter has a smooth outer cover with a compressible foam inner support. A locking collet is provided on the delivery catheter for securing the axial position of the coaptation member and delivery catheter on the flexible rail. Alternatively, the coaptation member has an outer cover of polycarbonate urethane with a flexible inner support holding the cover outward from the delivery catheter.

In either of the two previous systems, the ventricular anchor may comprise two separate anchors that cooperate to secure the flexible rail of the flexible rail to the ventricle tissue. In one version, the cover is tubular with both ends open, and if not made of polycarbonate urethane the cover is made of bioprosthetic tissue. If the flexible inner support is a compressible foam member it may substantially fill the cover and be an open cell foam that permits blood flow therethrough. The flexible inner support may also comprise a flexible frame with struts that extend substantially the length of the cover between the compressible foam member and the cover. Alternatively, the flexible frame has struts emanating from a central collar and engaging the inside of the cover. In one embodiment, wherein the cover is tubular with both ends open, while in another the cover is bell-shaped with a distal or ventricular side being open and a proximal or atrial side being closed. Alternatively, the cover is bell-shaped with both ends being closed.

A further understanding of the nature and advantages of the present invention are set forth in the following description and claims, particularly when considered in conjunction with the accompanying drawings in which like parts bear like reference numerals.

BRIEF DESCRIPTION OF THE DRAWINGS

To further clarify various aspects of embodiments of the present disclosure, a more particular description of the certain embodiments will be made by reference to various aspects of the appended drawings. It is appreciated that these drawings depict only typical embodiments of the present disclosure and are therefore not to be considered limiting of the scope of the disclosure. Moreover, while the figures may be drawn to scale for some embodiments, the figures are not necessarily drawn to scale for all embodiments. Embodiments of the present disclosure will be described and explained with additional specificity and detail through the use of the accompanying drawings.

FIG. 1A is a cutaway view of the human heart in a diastolic phase showing introduction of an anchoring catheter into the right ventricle as a first step in deploying a device of the present application for reducing tricuspid valve regurgitation;

FIG. 1B is a cutaway view of the human heart in a systolic phase showing retraction of the anchoring catheter after installing a device anchor at the apex of the right ventricle;

FIGS. 2A-2C are detailed views of installation of an exemplary device anchor by the anchoring catheter;

FIGS. 3A and 3B are sectional views of the right atrium and ventricle that illustrate deployment of a regurgitation

reduction device including a delivery catheter advanced along an anchor rail to position a coapting element within the tricuspid valve;

FIGS. 4A-4C are perspective and longitudinal sectional views of a locking collet shown proximally positioned on the catheter of FIGS. 3A and 3B that is used to fix the position of the delivery catheter and coapting element relative to the anchor rail;

FIG. 5 is a broader view of the final configuration of the regurgitation reduction device of the present application with a coapting element positioned within the tricuspid valve and a proximal length of the delivery catheter including the locking collet shown exiting the subclavian vein to remain implanted subcutaneously;

FIGS. 6A and 6B are assembled and exploded elevational views of an exemplary coapting element having an inner strut frame and tissue partially covering an atrial end of the coapting element;

FIGS. 7A and 7B are assembled and exploded elevational views of another coapting element having an inner strut frame and tissue partially covering a ventricular end of the coapting element;

FIG. 8 is an assembled elevational view of a still further coapting element having a tissue cover on the atrial end and cantilevered struts extending from the atrial end within the tissue cover;

FIGS. 9A-9C are assembled elevational and atrial end views of another coapting element with a tissue cover and cantilevered struts extending from the ventricular end thereof;

FIGS. 10A-10B are assembled elevational and ventricle end views of a coapting element having an atrial end tissue cover and an inner strut configuration with some struts extending the full length of the coapting element and some cantilevered from the atrial end;

FIGS. 11A-11B are views of a coapting element much like that shown in FIGS. 10A-10B but with the tissue cover and struts extending from the ventricular end;

FIG. 12 is an elevational view of a coaptation element much like FIG. 6A, but with a modified coupling structure on the proximal end of an inner mechanical frame that permits a delivery catheter to be snap fit thereto, and FIG. 12A is an enlargement of the proximal coupling;

FIG. 13 is an enlarged view of the proximal coupling between the delivery catheter and the mechanical frame of FIG. 12;

FIGS. 14A-14C are schematic views of various constructions of three-strut/three-panel coapting elements disclosed herein;

FIG. 15 is a schematic view of the construction of a two-strut/two-panel coapting element;

FIG. 16 is a schematic diagram of a representative coapting element and a pair of native tissue leaflets indicating certain key dimensions used in constructing the coapting element;

FIGS. 17A-17C are assembled and exploded views of a coapting element having a three-strut frame, a tubular tissue or other materials covering, and an inner compressible biocompatible material such as a foam;

FIG. 18 is an elevational view of the coapting element of FIGS. 17A-17C being inserted through a constrictor sleeve used for reducing the diameter of the coapting element during delivery into the body;

FIGS. 19 and 20 are assembled and exploded views, respectively, of an alternative coapting element comprising a bell-shaped polymer member held open at one end via a multi-strut frame;

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FIG. 21 is a partial cutaway perspective view of a coapting element similar to that shown in FIG. 19, but having a multi-strut frame which is positioned within the bell-shaped polymer member;

FIGS. 22A-22G illustrates an exemplary assembly sequence for the coapting element of FIGS. 19 and 21;

FIG. 23A is a perspective view of another coapting element of the present application wherein an outer biocompatible tubular cover mounts to an internal multiple strut frame and encloses a compressible member such as foam therein, and FIG. 23B is an end view thereof;

FIGS. 24A-24C and 25A-25B illustrate a number of components that comprise the coapting element of FIG. 23A;

FIGS. 26A and 26B are assembled and exploded views of a still further coapting element of the present application having an outer tubular cover surrounding a porous compressible member;

FIGS. 27A and 27B are assembled and exploded views of a coapting element similar to that in FIGS. 26 and 27 but wherein a ventricular end of the outer cover is closed;

FIG. 28 is an assembled view of a coapting element with an outer cover surrounding an inner compressible member and with a perforated inner catheter for removing air from the compressible member, shown, respectively, in FIGS. 29A and 29B;

FIG. 30 is a perspective view of a coapting element having an outer bell-shaped cover with a plurality of flow through holes on an otherwise closed atrial end, and FIGS. 31A and 31B show alternative hole patterns;

FIGS. 32A-32B are sectional views of the heart illustrating a regurgitation reduction device positioned in the right atrium/right ventricle and having a three-sided frame as a coapting element;

FIGS. 33A and 33B are elevational and end views of the coapting element from FIGS. 32A-32B;

FIGS. 34 and 35 are radial section views through the coapting element of FIG. 33A showing two different possible configurations, one hollow and one filled with a compressible material;

FIGS. 36A and 36B are sectional views of the heart in diastole and systole, respectively, showing a regurgitation reduction device which is mounted to the apex of the right ventricle with a spring that permits a coapting element to move in and out of the right ventricle in accordance with the cardiac cycle;

FIGS. 37 and 38 are views of alternative anchoring members utilizing coil springs;

FIG. 39 is a partial sectional view of an alternative anchoring device having concentric corkscrew anchors, while FIGS. 39A-39C illustrate steps in installation of the anchoring device;

FIGS. 40 and 41 are views of still further anchoring members of the present application;

FIGS. 42A and 42B show operation of a centering balloon that helps ensure proper positioning of an anchoring member at the apex of the right ventricle;

FIG. 43 illustrates a step in directing an anchoring catheter to the apex of the right ventricle using an L-shaped stabilizing catheter secured within a coronary sinus;

FIG. 44 schematically illustrates a stabilizing rod extending laterally from a regurgitation reduction device delivery catheter in the right atrium above the tricuspid valve;

FIG. 45 illustrates an adjustable stabilizing rod mounted on the delivery catheter and secured within the coronary sinus;

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FIG. 46 illustrates an alternative delivery catheter having a pivot joint just above the coapting element;

FIGS. 47A and 47B show two ways to anchor the delivery catheter to the superior vena cava for stabilizing the coapting element;

FIGS. 48A and 48B show a regurgitation reduction device having pull wires extending therethrough for altering the position of the coapting element within the tricuspid valve leaflets;

FIG. 49 shows a regurgitation reduction device anchored with stents in both the superior and inferior vena cava and having rods connecting the stents to the atrial side of the coapting element;

FIGS. 50A-50C are schematic views of a coapting element mounted for lateral movement on a flexible delivery catheter that collapses and allows rotation for seating centrally in the valve plane even if the delivery catheter is not central; and

FIGS. 51A and 51B are radial sectional views through the coapting element as seen in FIGS. 50A and 50B, respectively.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

The following description refers to the accompanying drawings, which illustrate specific embodiments of the invention. Other embodiments having different structures and operation do not depart from the scope of the present invention.

Exemplary embodiments of the present disclosure are directed to devices and methods for improving the function of a defective heart valve. It should be noted that various embodiments of coapting elements and systems for delivery and implant are disclosed herein, and any combination of these options may be made unless specifically excluded. For example, any of the coapting elements disclosed may be combined with any of the flexible rail anchors, even if not explicitly described. Likewise, the different constructions of coapting elements may be mixed and matched, such as combining any tissue cover with any inner flexible support, even if not explicitly disclosed. In short, individual components of the disclosed systems may be combined unless mutually exclusive or otherwise physically impossible.

FIGS. 1A and 1B are cutaway views of the human heart in diastolic and systolic phases, respectively. The right ventricle RV and left ventricle LV are separated from the right atrium RA and left atrium LA, respectively, by the tricuspid valve TV and mitral valve MV; i.e., the atrioventricular valves. Additionally, the aortic valve AV separates the left ventricle LV from the ascending aorta (not identified) and the pulmonary valve PV separates the right ventricle from the pulmonary artery (also not identified). Each of these valves has flexible leaflets extending inward across the respective orifices that come together or "coapt" in the flowstream to form the one-way fluid occluding surfaces. The regurgitation reduction devices of the present application are primarily intended for use to treat the atrioventricular valves, and in particular the tricuspid valve. Therefore, anatomical structures of the right atrium RA and right ventricle RV will be explained in greater detail, though it should be understood that the devices described herein may equally be used to treat the mitral valve MV.

The right atrium RA receives deoxygenated blood from the venous system through the superior vena cava SVC and the inferior vena cava IVC, the former entering the right atrium above, and the latter from below. The coronary sinus

CS is a collection of veins joined together to form a large vessel that collects deoxygenated blood from the heart muscle (myocardium), and delivers it to the right atrium RA. During the diastolic phase, or diastole, seen in FIG. 1A, the venous blood that collects in the right atrium RA is pulled through the tricuspid valve TV by expansion of the right ventricle RV. In the systolic phase, or systole, seen in FIG. 1B, the right ventricle RV collapses to force the venous blood through the pulmonary valve PV and pulmonary artery into the lungs. During systole, the leaflets of the tricuspid valve TV close to prevent the venous blood from regurgitating back into the right atrium RA. It is during systole that regurgitation through the tricuspid valve TV becomes an issue, and the devices of the present application are beneficial.

Regurgitation Reduction System:

FIGS. 1A and 1B show introduction of an anchoring catheter **20** into the right ventricle as a first step in deploying a device of the present application for reducing tricuspid valve regurgitation. The anchoring catheter **20** enters the right atrium RA from the superior vena cava SVC after having been introduced to the subclavian vein (see FIG. 5) using well-known methods, such as the Seldinger technique. More particularly, the anchoring catheter **20** preferably tracks over a pre-installed guide wire (not shown) that has been inserted into the subclavian vein and steered through the vasculature until it resides at the apex of the right ventricle. The physician advances the anchoring catheter **20** along the guide wire until its distal tip is touching the ventricular apex, as seen in FIG. 1A.

FIG. 1B shows retraction of a sheath **22** of the anchoring catheter **20** after installing a device anchor **24** at the apex of the right ventricle RV. The sheath **22** has desirably been removed completely from the patient's body in favor of the second catheter, described below.

First, a detail explanation of the structure and usage of an exemplary device anchor **24** will be provided with reference to FIGS. 2A-2C. FIG. 2A is an enlargement of the distal end of the anchoring catheter sheath **22** in the position of FIG. 1A. The device anchor **24** is seen within the sheath **22** positioned just within the distal end thereof. The device anchor **24** attaches to an elongated anchor rail **26**, which in some versions is constructed to have good capacity for torque. For instance, the anchor rail **26** may be constructed as a braided wire rod, or cable.

In FIG. 2B, the catheter sheath **22** is shown being retracted proximally, while the device anchor **24** and anchor rail **26** are expelled distally therefrom. The exemplary device anchor **24** includes a plurality of circumferentially distributed and distally-directed sharp tines or barbs **28** that pierce the tissue of the ventricular apex. The barbs **28** are held in a stressed configuration within the sheath **22**, and are provided with an outward elastic bias so that they curl outward upon release from the sheath. Desirably the barbs **28** are made of a super-elastic metal such as Nitinol. The outward curling of the barbs **28** can be seen in both FIGS. 2B and 2C, the latter showing the final relaxed configuration of the barbs. The operation to embed the device anchor **24** may be controlled under visualization, such as by providing radiopaque markers in and around the device anchor **24** and distal end of the catheter sheath **22**. Certain other devices described herein may be used to help position the device anchor **24** at the ventricular apex, as will be described. Although the particular device anchor **24** shown in FIGS. 2A-2C is considered highly effective, other anchors are

contemplated, such as shown and described below, and the application should not be considered limited to one type or another.

To facilitate central positioning of the anchor rail **26** during deployment the device is implanted with the assistance of a fluoroscope. For example, after properly positioning the patient so as to maximize the view of the target annulus, for example the tricuspid annulus, a pigtail catheter is placed in the right ventricle and contrast injected. This allows the user to see a clear outline of the annulus and the right ventricle. At this point, a frame of interest is selected (e.g., end systole) in which the annulus is clearly visible and the annulus to ventricular apex distance is minimized. On the monitor, the outline of the right ventricle, the annulus, and the pulmonary artery are traced. The center of the annulus is then identified and a reference line placed 90° thereto is drawn extending to the right ventricular wall. This provides a clear linear target for anchoring. In a preferred embodiment, the anchor **24** is preferably located in the base of the ventricle between the septum and the free wall.

Aligning the anchor rail **26** in this manner helps center the eventual positioning of a coapting element of the system within the tricuspid leaflets. If the coapting element is offset to the anterior or posterior side, it may get stuck in the tricuspid valve commissures resulting in leakage in the center of the valve. An alternative method is to place a device such as a Swan Ganz catheter through the right ventricle and into the pulmonary artery to verify that the viewing plane is parallel to the anterior/posterior viewing plane. Addition of a septal/lateral view on the fluoroscope may be important to center the anchor in patients that have a dilated annulus and right ventricle.

FIGS. 3A and 3B illustrate deployment of a regurgitation reduction device **30** including a delivery catheter **32** advanced along the anchor rail **26** to position a coapting element **34** within the tricuspid valve TV. The coapting element **34** fastens to a distal end of the delivery catheter **32**, both of which slide along the anchor rail **26**, which has been previously positioned as described above. Ultimately, as seen in FIG. 3B, the coapting element **34** resides within the tricuspid valve TV, the leaflets of which are shown closed in systole and in contact with the coapting element. Likewise, the delivery catheter **32** remains in the body as seen in FIGS. 3B and 5, and the prefix "delivery" should not be considered to limit its function. A variety of coapting elements are described herein, the common feature of which is the goal of providing a plug of sorts within the heart valve leaflets to mitigate or otherwise eliminate regurgitation. In the illustrated embodiment, the coapting element **34** includes an inner strut structure partly surrounded by bioprosthetic tissue, as will be described in more detail below.

A locking mechanism is provided on the regurgitation reduction device **30** to lock the position of the coapting element **34** within the tricuspid valve TV and relative to the fixed anchor rail **26**. For example, a locking collet **40** along the length of the delivery catheter **32** permits the physician to selectively lock the position of the delivery catheter, and thus the connected coapting element **34**, on the anchor rail **26**. There are of course a number of ways to lock a catheter over a concentric guide rail, and the application should not be considered limited to the illustrated embodiment. For instance, rather than a locking collet **40**, a crimpable section such as a stainless steel tube may be included on the delivery catheter **32** at a location near the skin entry point and spaced apart from the location of the coapting element **34**. The physician need only position the coapting element **34** within

the leaflets, crimp the catheter **32** onto the anchor rail **26**, and then sever both the catheter and rail above the crimp point.

Details of the exemplary locking collet **40** are seen in FIGS. 4A-4C. The collet **40** includes two short tubular grips **42a**, **42b** that are internally threaded and engage a common externally threaded tubular shaft member **44**. The delivery catheter **32** is interrupted by the collet **40**, and free ends of the catheter fasten within bores provided in opposite ends of the grips **42a**, **42b**. As seen in FIG. 4B, the anchor rail **26** extends through the middle of the locking collet **40**, thus continuing the length of the delivery catheter **32**. Furthermore, when the grips **42a**, **42b** are separated from each other as seen in FIGS. 4A and 4B, the anchor rail **26** slides freely through the locking collet **40**.

An inner, generally tubular wedge member **46** is concentrically positioned between the shaft member **44** and the anchor rail **26**. One or both ends of the wedge member **46** has a tapered surface **48** (see FIG. 4C) that interacts with a similarly tapered inner bore of the surrounding tubular grip **42a**, **42b**. The wedge member **46** features a series of axial slots extending from opposite ends which permit its diameter to be reduced from radially inward forces applied by the surrounding grips **42a**, **42b** and shaft member **44**. More particularly, FIG. 4C shows movement of the two grips **42a**, **42b** toward each other from screwing them together over the threaded shaft member **44**. Desirably, outward ribs or other such frictional enhancers are provided on the exterior of both of the grips **42a**, **42b** to facilitate the application of torque in the often wet surgical environment. Axial movement of the tapered inner bore of one or both of the grips **42a**, **42b** forces inward the tapered surface **48** of the wedge member **46**, and also the outer ends of the shaft member **44**. In other words, screwing the grips **42a**, **42b** together cams the shaft member and a wedge member **46** inward. The dimensions are such that when the two grips **42a**, **42b** come together, the inward force applied by the wedge member **46** on the anchor rail **26** is sufficient to lock the delivery catheter **32** and anchor rail.

Now with reference to FIG. 5, the entire regurgitation reduction device **30** can be seen extending from the apex of the right ventricle RV upward through the superior vena cava SVC and into the subclavian vein SV. A proximal length of the delivery catheter **32** including the locking collet **40** exits the subclavian vein SV through a puncture and remains implanted subcutaneously; preferably coiling upon itself as shown. In the procedure, the physician first ensures proper positioning of the coapting element **34** within the tricuspid valve TV, then locks the delivery catheter **32** with respect to the anchor rail **26** by actuating the locking collet **40**, and then severs that portion of the delivery catheter **32** that extends proximally from the locking collet. The collet **40** and/or coiled portion of the delivery catheter **32** may be sutured or otherwise anchored in place to subcutaneous tissues outside the subclavian vein SV. It is also worth noting that since the delivery catheter **32** slides with respect to the anchor rail **26**, it may be completely removed to withdraw the coapting element **34** and abort the procedure—either during or after implantation. The implant configuration is similar to that practiced when securing a pacemaker with an electrode in the right atrium muscle tissue and the leads extending to the associated pulse generator placed outside the subclavian vein. Indeed, the procedure may be performed in conjunction with the implant of a pacing lead.

Coapting Elements:

As mentioned, a number of different coapting elements are described in the present application. Indeed, the present

application provides a plurality of solutions for preventing regurgitation in atrioventricular valves, none of which should be viewed as necessarily more effective than another. For example, the choice of coapting element depends partly on physician preference, partly on anatomical particularities, partly on the results of clinical examination of the condition of the patient, and other factors.

One broad category of coapting element that is disclosed herein and has been subject to testing is a flexible mechanical frame structure at least partially covered with bioprosthetic tissue. The inner frame structure is flexible enough to react to the inward forces imparted by the closing heart valve leaflets, and therefore undergo a shape change to more completely coapt with the leaflets, thus reducing regurgitant jets. The bioprosthetic tissue covering helps reduce material interactions between the native leaflets and the inner mechanical frame. As mentioned above, the regurgitation reduction device can be effectively deployed at either the tricuspid or mitral valves, the former which typically has three leaflet cusps defined around the orifice while the latter has just two. The tissue-covered mechanical frame structure thus represents an effective co-optation element for both valves by providing a highly flexible structure which is substantially inert to tissue interactions.

An exemplary embodiment of this so-called “Flexible Bell Coaptation Element” consists of a pericardial tissue (or a biocompatible flexible material) that is cut and sewn to create a sac/bell shape that is able to hold liquid (blood). One embodiment is designed to sit in the valve plane such that the open end is towards the atrium and the closed portion towards the ventricle. Therefore during diastole, blood flows into the coaptation element and fills the sac, conversely during systole as the native leaflets begin to close and contact the coaptation element, the pressure and blood flow work to decrease the size of the coaptation element by pushing blood out of the top edge sufficiently while still creating a seal.

Variations on the system include various design shapes at the ventricular end that is closed such as a half circle, triangle, ellipse or the like. Additionally sutures on the closed end as well as axially along the coaptation element better define how the element closes from interaction with the native leaflets. Lastly a more rigid support such as cloth, wire or other material could be sutured along the open atrial seated edge to ensure that the design remained open during the cardiac cycle. These principles apply equally to coapting elements that are open to the ventricle and closed to the atrium.

FIGS. 6A and 6B are assembled and exploded elevational views of an exemplary coapting element **34** having an inner strut frame **50** and a tissue cover **52** partially covering an atrial end of the coapting element. For the sake of uniformity, in these figures and others in the application the coapting elements are depicted such that the atrial end is up, while the ventricular end is down. These directions may also be referred to as “proximal” as a synonym for up or the atrial end, and “distal” as a synonym for down or the ventricular end, which are terms relative to the physician’s perspective.

A small portion of the delivery catheter **32** is seen at the proximal end of the coapting element **34**. In one embodiment, a short tubular collar **54** fastens to the distal end of the delivery catheter **32** and provides structure to surround the proximal ends of a plurality of struts **56** that form the strut frame **50**. A second tubular collar **58** holds together the distal ends of the struts **56** and attaches to a small ferrule **60** having a through bore that slides over the anchor rail **26**. Each of the struts **56** has proximal and distal ends that are formed as a

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part of (or constrained within) these collars **54**, **58** and a mid-portion that arcs radially outward to extend substantially parallel to the axis of the coapting element **34**. The frame shape is thus a generally elongated oval. In the illustrated embodiment, there are six struts **56** in the frame **50**, although more or less could be provided. The struts **56** are desirably formed of a super-elastic material such as Nitinol so as to have a minimum amount of rigidity to form the generally cylindrical outline of the frame but maximum flexibility so that the frame deforms from the inward forces imparted by the heart valve leaflets.

The tissue cover **52** preferably comprises one or more panels **61** of bioprosthetic tissue sewn around the struts **56** of the frame **50**. A single axial seam **62** is shown in the figures, though as will be explained below the cover **52** is typically formed of two or three panels sewn together with a matching number of seams. The tissue cover **52** may be formed of a variety of xenograft sheet tissue, though bovine pericardial tissue is particularly preferred for its long history of use in cardiac implants, physical properties and relative availability. Other options are porcine or equine pericardium, for example. In the embodiment illustrated in FIGS. **6A-6C**, the tissue cover **52** has a proximal end that is closed to fluid flow, and a distal end **64** that is open; thus, the cover resembles a bell shape. Desirably, the axial length of the cover **52** extends from the proximal collar **54** approximately three-quarters of the way down to the distal collar **58**, to the end of the flat section of the device. As mentioned above, the open bell shape desirably facilitates functioning of the coapting element. Namely, during diastole, blood flows around the coaptation element **34**, while during systole, as the native leaflets close and contact the coaptation element, the pressure and blood flow work to fill the interior of the coaptation element by pushing blood in, the interior of the coaptation element is at the same pressure as the RV and a seal is created. These phases of the cardiac cycle are common to both the tricuspid and mitral valves. Generally the coaptation elements that are closed on the atrial side and open to the ventricular side move essentially like a parachute—filling in systole, and blood flowing around without collapse in diastole.

FIGS. **7A** and **7B** illustrate an alternative coapting element **68** much like the coapting element **34** described above, having an inner strut frame **70** and a tissue cover **72** partially covering a ventricular end of the coapting element, which functions like a flexible cup to block regurgitation. Indeed, the structure of the coapting element **68** is identical to that described above except for two features—the tissue cover **72** is closed at the ventricular end, but open at the atrial end, and there are three elongated struts **74** extending between and captured by upper and lower collars **76a**, **76b**. The number of struts can vary for both designs, though 6 or 9 struts are currently contemplated. Once again, the delivery catheter **32** fixes to the upper collar **76a**, while the anchor rail **26** extends through the entire structure and slides through the lower collar **76b**. After implant of the upwardly opening coapting element **68**, blood will close the tricuspid valve leaflets during systole around the tissue cover **72** (as in FIG. **3B**) with relatively little resistance from the coapting element. Conversely, during diastole blood flows downward from the right atrium to the right ventricle around the coapting element **68**, and though some will flow into and inflate the tissue cover **72**, its size will not significantly impede filling of the right ventricle.

FIG. **8** is an assembled elevational view of a still further coapting element **80** having a tissue cover **82** on the atrial end (open to the ventricle) and cantilevered struts (not

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visible) extending from the atrial end within the tissue cover. That is, the coapting element **80** is similar to coapting element **34** from FIG. **6A**, though instead of an oval-shaped mechanical frame within the tissue cover **82**, the struts are simply fixed to and cantilevered from an atrial collar **86**. As before, the delivery catheter **30** attaches to the collar **86**, and the entire assembly slides over the anchor rail **26**.

FIGS. **9A-9C** illustrate another coapting element **90** with a tissue cover **92** open to the atrial end and cantilevered struts **94** extending from a collar **96** at the ventricular end. In other words, the coapting element **90** is essentially an inverse to the coapting element **80** of FIG. **8**. FIG. **9B** shows the coapting element **90** looking down from the atrial side in an expanded configuration of the tissue cover **92** in diastole when blood flows downward from the right atrium to the right ventricle and inflates the cover. In FIG. **9C**, systolic pressures in the right ventricle close the tricuspid valve leaflets around the coapting element **90**, thus causing it to collapse and force blood from the interior of the tissue cover **92** into the right atrium. It will be noticed that some of the struts **94** collapse inward more than others, reflecting the uneven inward forces imparted by the tricuspid leaflets. Struts that do not deform so much remain bowed outward toward the valve commissures. The diagram is schematic, and shown with three struts moving all the way in and three remaining in approximately the same position. However, it will be understood that the compacted shape of the coapting element **90** will be relatively random, and may change from cycle to cycle.

FIGS. **10A-10B** shows a still further embodiment of a coapting element **100** having an atrial end tissue cover **102**, similar to that shown in FIGS. **6A** and **8**, but with an inner strut configuration with some struts **104** extending the full length of the coapting element and some struts **106** cantilevered from the atrial end, in particular from an atrial collar **108**. The staggered nature of the full-length struts **104** and cantilevered struts **106** is seen from the ventricular end in FIG. **10B**. With this configuration, segments of the coapting element **100** having the cantilevered struts **106** are more inwardly flexible than the segments having the full-length of struts **104**, which provides a collapsible structure that is someone more flexible than the embodiment of FIG. **6A** but more rigid than the embodiment shown in FIG. **8**.

FIGS. **11A-11B** illustrate a similar coapting element **110** as in FIGS. **10A-10B**, but with the tissue cover **112** and struts **114**, **116** extending from the ventricular end, preferably from a ventricular collar **118**.

Many of the coapting elements described herein benefit from the use of a bioprosthetic tissue covering. Often, such tissue coverings must be stored in a preservative solution, such as glutaraldehyde, for long periods, which may be deleterious to the material of the synthetic components of the overall device. Accordingly, any of the bioprosthetic tissue coapting elements described herein should be stored separately from other components that could be damaged from long-term storage and preservative solution, such as polymer catheters and the like.

FIGS. **12**, **12A**, and **13** illustrate one such arrangement where a coapting element **120** has a proximal coupling sleeve **121** that can be snap fit to a distal coupler **122** of a delivery catheter. More particularly, FIGS. **12A** and **13** show small oval windows **123** in the coupler **122** which received outwardly biased spring tabs **124** on a tubular hub **125** of the coupling sleeve **121**. At the time of the surgical procedure, a technician in the operating room removes the bioprosthetic coapting element **120** from its liquid-filled storage container, typically rinsing it, and then joins the catheter coupler **122**

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to the proximal sleeve **121** by pushing the two together until the tabs **124** spring outward through the windows **123**. It should be also noted that the internal mechanical frame structure including the flexible struts **126** are formed in one homogenous piece with the tubular hub **125** of the coupling sleeve **121**, which improves long-term integrity of the entire structure.

As mentioned above, a preferred construction of the mechanical frame/tissue cover coapting elements includes a plurality of panels of bioprosthetic tissue sewn to the inner struts. FIGS. **14A-14C** schematically illustrate several different configurations of three-strut/three-panel coapting elements in this regard. More particularly, FIG. **14A** shows the three panels **128** of bioprosthetic tissue having generally rectangular configurations except for their lower ends which are pointed. A view of the finished coapting element from its open end is seen to the right wherein all of the six struts **130** are cantilevered from the closed end. In a preferred construction, cloth pieces **132** are first sewn around some or all of the struts **130**. Separately, the three tissue panels **128** are sewn to each other to form a tubular structure, and such that the flaps of the longitudinal seams face to the inside of the tube. This may require first sewing the seams on the outside and then inverting the tubular structure. Subsequently, the tubular structure of the three panels **128** is sewn to the cloth pieces **132** preassembled around some or all of the struts. In the illustrated embodiment, there are three panels **128** and thus three seams, so that only three cloth pieces **132** are used around three of the six struts **130**. Finally, the pointed lower ends of the tissue panels **128** are sewn together to close off that end, whether it be the atrial or ventricular side.

FIG. **14B** is much the same as the construction of FIG. **14A**, however the mechanical frame structure has six struts **134** that extend the full length of the coapting elements with none of them cantilevered. Finally, FIG. **14C** shows another similar embodiment wherein there are three struts **136** extending the full length of the coapting element, with three intermediate struts **138** cantilevered from the closed end of the mechanical frame.

FIG. **15** schematically illustrates components in the construction of a two-strut/two-panel coapting element. Because of the modified three-dimensional shape, the lower ends of the panels **140** are curved rather than pointed. The two struts **142** extend the full length of the coapting element and are diametrically opposed. This coapting element thus has a much more two-dimensional shape, though the open end of the tissue cover permits the structure to be inflated when the element is pressurized from the open end.

FIG. **16** is a schematic diagram of a pair of native tissue leaflets **144** indicating certain key dimensions used in constructing the coapting element. The inquiry seeks to determine a preferred height of the coapting element, or at least the height of the leaflet contacting surface of the elements. It is known that the length of heart valve leaflets are often mismatched, and the dimension LM indicates the leaflet mismatch as a distance along the axis of the valve. An axial dimension of a coapting element that fits within these two mismatched leaflets will therefore have a minimum height that starts at the tip of the longer leaflet and extends upward approximately twice the leaflet mismatch LM dimension, indicated as H_{min} . To avoid inserting too large a structure between the leaflets, a dimension H_{max} extends from approximately the plane of the annulus of the leaflets (i.e., where they attach to the surrounding wall) down to a distance into the ventricle which is centered at the center of the dimension H_{min} . The leaflet excursion LE reflects the length along which the leaflets are known to contact the

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coapting devices. That is, the leaflets first hit the device and then move down with the contraction of the heart. There must therefore be enough surface length or leaflet excursion LE for the leaflets to maintain contact. In general, the axial dimension of the coapting element should ensure enough coaptation length to accommodate leaflet mismatch and leaflet excursion without protruding too much into the ventricle or atrium.

FIGS. **17A-17C** illustrate another coapting element **150** having a three-strut mechanical frame **152**, a tubular tissue covering **154**, and an inner foam cylinder **156**. The foam cylinder **156** has a through bore for receiving a delivery catheter **158**. Three struts **160** are retained by a pair of end collars **162** secured to the delivery catheter **158**. As described above, the tissue covering **154** desirably includes a plurality, typically three, of rectangular panels that are sewn together and then sewn to a cloth covering surrounding each of the struts (not shown). The resulting structure of the coapting element **150** is compressible, though the inner foam cylinder **156** expands in its relaxed configuration to provide a generally continuous curved outer surface for good contact with the surrounding heart valve leaflets.

FIG. **18** illustrates one technique for compressing the coapting element **154** for introduction into a patient's vasculature, such as into a patient's subclavian vein. A generally funnel-shaped introducer **170** has a wide proximal end **172** and a much smaller distal end **174**, with the diameter either stepping down intermittently along its length or continuously. By pushing the delivery catheter and ultimately the coapting element **150** into the introducer **170** from its proximal end **172**, the coapting element can be gradually compressed until it fits through the narrow distal end **174**. The distal end **174** may be inserted directly into the subclavian vein, or may connect to a pre-inserted delivery sheath of approximate the same diameter.

FIGS. **19** and **20** illustrate an alternative coapting element **180** comprising a bell-shaped polymer member **182** held open at one end via a multi-strut frame **184**. An upper or atrial collar **186** connects both to the polymer member **182** and to a delivery catheter **30**, although the polymer member may be connected directly to the delivery catheter such as via heat bonding. The delivery catheter **30** extends through the interior of the polymer member **182** and rides over the anchor rail **26**, as before. The multi-strut frame **184** includes a ventricular collar **188** that attaches to the delivery catheter **30** and has a plurality, preferably three, struts **190** that angle outward therefrom in a proximal or atrial direction and terminate in small pads or feet **192**. The feet **192** attach to an inner surface of a distal or ventricular reinforcing band **194** on the bell-shaped polymer member **182**. The struts **190** are resilient such that the feet **192** apply radial outward forces to the band **194** so as to maintain the distal end of the polymer member **182** open.

FIG. **21** is a partial cutaway perspective view of a coapting element **180'** similar to that shown in FIG. **19**, but having a multi-strut frame **184'** which is positioned within the bell-shaped polymer member **182**. The delivery catheter **30** may extend just past the ventricular collar **188'** or farther down into the ventricle as shown, such as to provide an expansion balloon to assist in guiding the anchor rail **26** to a proper anchoring position, as will be described below.

Both the coapting elements **180** and **180'** include relatively square closed ends **196** of the polymer members **182**, **182'**. This is believed to be beneficial to avoid elongated narrow internal spaces where blood might stagnate and perhaps coagulate. A preferred material for the polymer members **182**, **182'** is a polycarbonate urethane (Carbothane

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from Lubrizol, Bionate from DSM, ChronoFlex from Advansource) which has extremely good durability over long periods of time, as opposed to materials such as Nylon used for typical catheter balloons. Alternatively, a polycarbonate silicone may also be used. In one embodiment, the outside diameter of the polymer members **182**, **182'** is about 10 mm, while the inside diameter of the neck that attaches to the delivery catheter **30** is about 0.10 inches (2.54 mm), and the constant diameter tubular portion is around 25 mm.

FIGS. **22A-22G** illustrates an exemplary assembly sequence for the coapting element **180** and **180'** of FIGS. **19** and **21**. First, a polycarbonate urethane balloon **198** having substantially square ends seen in FIG. **22A** is cut to length to result in the open-ended polymer member **182** in FIG. **22B**. Subsequently, a band **184** of polymer reinforcing material is he bonded to the open end of the polymer member **182**. The reinforcing material may be made of the same material as the polymer balloon but in a thicker extrusion. In one embodiment, the reinforcing band **192** is also radiopaque to provide visibility of the open end of the device. Subsequently, as seen in FIG. **22D**, a neck portion of the polymer member **182** is heat bonded to the delivery catheter **30**, or via an atrial collar as shown in FIGS. **19** and **21**. FIGS. **22E** and **22F** show attachment of the feet **192** of the frame **184** to the reinforcing band **194**. The feet **192** may be attached in a number of ways, including heat bonding, adhesive, or even via sutures. FIG. **22G** shows a version where small sutures **199** are used to secure the feet **192** of the frame **184** to the band **194**.

FIG. **23A** is a perspective view of another coapting element **200** having an outer biocompatible tubular cover **202** mounted to an internal multiple strut frame **204** and enclosing a compressible member **206** such as foam therein. In a preferred embodiment, the tubular cover **202** comprises bioprosthetic tissue, such as bovine pericardial tissue, although other biocompatible materials such as the polycarbonate urethane described above could be used. FIG. **23B** is an end view of the coapting element **200** illustrating the annular compressible member **206** surrounding the central delivery catheter **30**, and showing the inset position of a plurality of longitudinal struts **208** that make up the frame **204**. The delivery catheter **30** slides over the anchoring rail **26**. As seen in FIG. **23A**, the frame **204** includes an atrial collar **210** from which the struts **208** extend outward and then longitudinally approximately the entire length of the coapting element **200**. The struts **208** are not joined at the distal end so as to be cantilevered from the collar **210**. The collar **210** may attach via a snap-fit to a distal coupler **212** connected to the delivery catheter **30**, much like the coupling sleeve **121** and distal coupler **122** described above with respect to FIG. **13**.

FIGS. **24A-24C** and **25A-25B** illustrate a number of components forming the coapting element **200**. A subassembly of the frame **204** is shown secured to three panels **214** that make up the tubular cover **202**. In particular, the frame **204** defines a tripod shape with three struts **208** each of which extends along and defines a junction between adjacent panels **214**. The coapting element **200** is relatively flush and cylindrical on its outer surface, with the struts **208** being inset therefrom. FIG. **24B** shows the frame **204** isolated with fabric tubes **216** sewn to the longitudinal portion of the struts **208**. FIG. **24C** is a detail of the junction between the struts **208** and adjacent panels **214**, wherein each panel includes an inwardly-directed edge which flanks the strut and is secured thereto via a number of sutures **218**. The inset struts **208** and seam between the panels **214** are received in longitudinal outer grooves **219** formed in the compressible member **206**,

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as seen in FIGS. **25A** and **25B**. As mentioned there are preferably three struts **208**, but more or less could also be used. Furthermore, the compressible member **206** as an overall cylindrical outer profile, which substantially defines the final shape of the coapting element **200**, but other cross-sectional shapes such as oval or rounded triangular may also be utilized.

As mentioned, the panels **214** of the tubular cover **202** are desirably bioprosthetic tissue, such as bovine pericardium. In a preferred embodiment, a smooth side of the pericardium is placed facing outward so as to render the exterior of the coapting element **200** smooth as well. As is well known, pericardium typically has a smooth side and a fibrous or rough side. The frame **204** is desirably highly flexible, such as being formed of Nitinol. The resulting coapting element **200** is highly compressible, thus responding to the forces imparted thereon by the surrounding valve leaflets and easily conforming so as to best prevent regurgitation.

FIG. **26A** shows another coapting element **220** assembled, while FIG. **26B** shows the individual components thereof exploded. The coapting element **220** includes an outer tubular cover **222** surrounding a porous compressible member **224**, and has a proximal frame **226** connected between a proximal end of the tubular cover and a delivery catheter **30**. The tubular cover **222** is desirably formed of a polycarbonate urethane. The frame **226** may be similar to those described above, having a tripod-shaped series of struts that terminate in feet **228** attached to a reinforcing or radiopaque band **230**. The porous compressible member **224** is desirably formed of an open cell foam which enables a small amount of blood flow therethrough. An open cell foam polycarbonate urethane provided by Biomerix of Fremont, Calif. may be desirable. Permitting slight blood flow through the coapting element **220** may help prevent stagnation and possible coagulation. Alternatively, the inner compressible member **224** may be a blood-impermeable foam, or an open cell foam covered with an impermeable layer.

FIGS. **27A** and **27B** are assembled and exploded views of a coapting element **230** similar to that in FIGS. **26A** and **26B** but wherein an outer cover **231** is bell-shaped with a closed ventricular end **232** and no supporting frame. The outer cover **231** is desirably a polycarbonate urethane, and preferably includes a radiopaque band **233** surrounding its proximal or atrial end.

FIG. **28** shows a coapting element **234** with an outer generally bell-shaped cover **235** surrounding an annular compressible member **236** mounted around an inner catheter **237** having perforations **238** for adding and removing air from the compressible member. As before, the inner catheter **237** slides over a flexible rail **26**. The flow arrows in FIGS. **29A** and **29B** show the injection and aspiration of air, respectively, from the inner catheter **237** to and from the compressible member **236**, which is desirably an open cell foam. In this way, the size of the coaptation element **234** may be reduced for delivery and increased after implant. The cover **235** thus functions something like a balloon, and is desirably formed of Carbothane. The catheter **237** is also made of Carbothane so that the distal and proximal necks of the cover **235** can easily be heat bonded thereto for a good seal, and is desirably reinforced to provide good inner support for the pressures generated within the cover **235**.

FIG. **30** is a perspective view of a still further coapting element **240** having an outer bell-shaped cover **242** with a plurality of flow through holes **244** on an otherwise closed atrial end **246**. A flexible frame **248** including a tripod of struts **250** maintains the distal or ventricular end open. FIGS. **31A** and **31B** show alternative hole patterns, which should

not be considered limiting. For example, a circular array of round holes **244** as in FIG. **31A** may be provided, or the pattern may be a regular distribution of non-circular such as rectangular through holes **254** as in FIG. **31B**. The through holes **244**, **254** are intended to permit a small amount of seepage through the otherwise closed end **246** of the coaptation element **240**, thus helping to avoid stagnation and coagulation of the blood.

FIGS. **32A-32B** illustrate a regurgitation reduction device **280** positioned in the right atrium/right ventricle having a three-sided frame **282** as a coaptation element, and FIGS. **33A** and **33B** show greater detail of the coaptation element. FIG. **32A** shows the heart in diastole during which time venous blood flows into the right ventricle between the open tricuspid valve leaflets and the three-sided frame **282**. In the systolic phase, as seen in FIG. **32B**, the tricuspid leaflets close around the compressible frame **282**, thus coapting against the frame and eliminating openings to prevent regurgitation.

FIG. **33B** shows the desirably three-sided radial profile of the frame **282**, with three relatively flat convex sides **284** separated by rounded corners **286**. This rounded triangular shape is believed to faithfully conform to the three tricuspid leaflets as they close, this better preventing regurgitation. Moreover, the frame **282** is desirably under-filled with fluid so that it can be compressed and deformed by the leaflets. FIG. **33A** also shows a preferred longitudinal profile of the frame **282**, with an asymmetric shape having a gradually overall longitudinal curvature **287** and an enlarged belly region **288** just distal from a midline. The shape resembles a jalapeno pepper. Due to the curvature of the path from the superior vena cava SVC down through the tricuspid valve TV and into the right ventricle RV, the overall curvature **287** of the frame **282** helps position a mid-section more perpendicular to the tricuspid valve leaflets, while the uneven longitudinal thickness with the belly region **288** is believed to more effectively coapt with the leaflets.

As an alternative to being fluid-filled, the frame **282** may have a plurality (e.g. >20) of very thin and highly flexible struts (not shown) that connect between top and bottom collars, for instance. The struts thus relocate independently of one another, which allows leaflet motion to deform the highly compliant frame **282** into whatever shape best conforms to the remaining orifice. Since segments of the frame **282** adjacent areas with high leaflet mobility would be compressed, the coaptation element could be dramatically oversized with respect to the regurgitant orifice size in order to maintain coaptation in commissural regions.

FIGS. **34** and **35** are radial section views through the coaptation element **280** of FIG. **33A** showing two different possible configurations. In a first embodiment in FIG. **34**, the coaptation element **280** is hollow or filled with a fluid such as saline. In a second embodiment in FIG. **35**, the coaptation element **280** has a compressible member **290** interposed between an outer cover **284** and the delivery catheter **30**. The compressible member **290** may be an open cell polycarbonate urethane foam, for example. Likewise, the outer cover may be a polycarbonate urethane. The latter configuration eliminates the potential for the fluid-filled frame **282** to deflate, thus maintaining good coaptation function for extended periods.

One potential challenge of a static coaptation element within the tricuspid valve annulus could be diastolic stenosis, i.e. restriction of blood flow from the right atrium to the right ventricle during diastole. In patients with an excessively large regurgitant orifice, sizing the device for proper coaptation during systole could have consequences in dias-

tole. To address this issue, a coaptation element **300** could be attached to a flexible metallic spring **304** connected to anchor **302**, therefore allowing the coaptation element to move in and out of the annulus plane during systole and diastole, respectively (see FIGS. **36A** and **36B**). During systole, as in FIG. **36B**, the pressure gradient as well as fluid inertial forces would cause the spring **304** to extend, and during diastole the spring constant as well as fluid inertial forces would cause the spring to contract. Instead of just one spring distal to the coaptation element, a spring could be placed on both sides in order to increase mobility. Alternatively, with one spring, the "home" position of the coaptation element (i.e. with no force from the spring or fluid) could either be at the annulus plane or below the annulus plane in the RV. In the former case, inertial forces of diastolic flow would be required to move the coaptation element down out of the annulus plane during diastole, and in the latter case, both inertial forces of systolic flow and forces from the RV/RA pressure gradient could move the coaptation element up to the annulus during systole.

Anchors and Alternative Anchor Placement:

The following list of embodiments presents additional design ideas for the catheter railing and anchoring system:

FIGS. **37** and **38** are views of alternative anchoring members utilizing conical coil springs. One potential challenge of some proposed helical anchors is the limited surface area on which the anchor can "grab" tissue given its short cylindrical length (2 mm). In order to maximize the area of tissue contact over the 2 mm length of the anchor, a modified helical anchor **310** could be developed which has a conical shape, i.e. a circular cross-section of increasing size towards the distal end. The conical spring anchor **310** could be provide at the end of an anchor rail **312**, as previously described. Such an anchor design could increase retention force by increasing the cross-sectional area of contact between the anchor coil and the tissue. Additionally, as the initial cut of the anchor **310** into the tissue would be largest followed by decreasing coil diameter as the anchor is screwed in, the anchor could effectively "cinch" in a volume of tissue into a compacted space. Such a feature could potentially minimize the risk for anchor tear-out by increasing the local tissue density at the anchor site. The conical spring **310** could be comprised of any shape memory material capable of collapsing or wrapping down to a smaller constant diameter to fit through a catheter lumen, then capable of expanding to the natural conical shape upon exiting the delivery sheath into the RV.

Alternatively, a conical anchor **314** could be connected via an elongated helical section **316** at its proximal end designed to remain in the RV (not screwed into the tissue but directly next to it), such as shown in FIG. **38**. The elongated helical section **316** provides shock absorption capabilities against compressive/tensile stresses, thus reducing tear-away stresses on the RV apex, and also flexibility capabilities under bending stresses.

Using helical structures for anchoring the devices described herein in the right ventricle holds a number of advantages (e.g. ease of delivery, acute removability, minimal tissue damage, etc.). However, one potential challenge could be the tendency of a helical structure to "unscrew" itself out of the tissue, either acutely or over time due to the contractile motions of the ventricle. To address this issue, an anchor system in FIG. **39** includes concentric corkscrew anchors; an inner anchor **320** at the end of an inner tube **322**, and an outer anchor **324** on the end of an outer tube **326**. FIGS. **39A-39C** illustrate steps in installation of the anchoring device, in which first the inner anchor **320** having a

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clockwise orientation is screwed into the tissue. Next, the slightly larger second anchor **324**, having a counterclockwise orientation, and its tube **326** slide over the first anchor **320** and tube **322** and screws into the tissue in the opposite direction. Finally, the two anchors could be fixed together with a locking mechanism (e.g., pin-through-hole style). The resulting structure would resist unscrewing out of the tissue, since each helical coil opposes the twisting motion of the other.

FIG. **40** shows another configuration with a helical corkscrew-type anchor **330** on the end of a tube **332**, and a pair of struts **334** that may be independently expelled from the distal end of the tube into contact with the tissue surrounding the anchor. Rather than screwing in a second relatively similar anchor in the opposite direction to prevent twist-out, the struts **334** pass through the tube lumen and extend outwards in an L-shaped manner to provide an anti-rotation anchor to the device. These struts **334** should be thick enough to press against the RV apex tissue and apply friction thereto to prevent twisting motion of the anchor **330**.

In an alternative approach to enabling fine control over the position of the coaptation element within the valve plane, as seen in FIG. **41**, a series of two or more anchors **340** could be deployed in various areas of the RV (including possibly the papillary muscles). The attached anchor rails **342** could all extend through a lumen of the coaptation element (not shown). In order to re-position the coaptation element, the tension on any given anchor rail **342** could be altered independently at the access site, thus increasing or decreasing the degree of tethering on the coaptation element in a certain direction. For example, to move the coaptation element to a more posterior position within the valve, the anchor rail **342** corresponding to the more posterior anchor **340** could be pulled more taught. Once the desired position is achieved, the relative lengths of all the anchor rails could be fixed with respect to the coaptation element catheter via a locking or clamping mechanism at the proximal end of the device. The anchor rails referenced previously could instead be cable wires (with no lumen) in order to minimize the profile of the coaptation element catheter given that multiple anchor attachments will need to fit within the device inner lumen. In order to facilitate easily distinguishing which cable attaches to which anchor, the catheter could contain a series of lumens (at least two) for cable wires which would be labeled based on anatomical location of the corresponding anchor. Therefore, at the proximal end of the device, it would be clear which cable would be required to pull in order to translate the coaptation element in a certain direction.

FIGS. **42A** and **42B** show operation of a centering balloon **350** that helps ensure proper positioning of an anchor **352** at the apex of the right ventricle. A series of experiments in a bench-top pulsatile flow model with porcine hearts has emphasized the importance of RV anchor position for achieving central location of the coaptation element within the valve. Thus, it may be necessary to utilize an accessory catheter **354** for the present device to help facilitate delivery of the anchor **352** to the ideal location within the ventricle, or the centering balloon **250** may be mounted on the distal end of the delivery/anchoring catheter itself. One such approach relies on using the annulus itself to guide the anchor shaft. For instance, a perfusion balloon **350** large enough to fill the entire valve could be inflated within the tricuspid annulus, therefore counting on opposition between the annulus and the perfusion balloon to orient the angle of the catheter lumen directly normal to and through the center of the valve plane. FIG. **42A** shows the unwanted position of

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the anchor **350** before balloon inflation, while FIG. **42B** shows the desired positioning at the RV apex after the balloon **350** is inflated. At this point, the anchor shaft would pass through the lumen of the perfusion balloon catheter (either an accessory catheter or the delivery catheter itself), which is oriented so as to guide the anchor to the ideal central location along the anterior-posterior axis of the RV apex. The centering balloon **250** allows the delivery system to track into the RV while avoiding chords and ensuring central placement rather than between leaflets.

FIG. **43** illustrates a step in directing an anchoring catheter **360** to the apex of the right ventricle using an L-shaped stabilizing catheter **362** secured within a coronary sinus. This configuration addresses the challenge of guiding the anchor delivery. The catheter **362** is capable of deflecting into an L-shape, and would be advanced from the SVC, into the right atrium, then into the coronary sinus, which would provide a stabilizing feature for the guide catheter. The catheter **362** could be maneuvered further in or out of the coronary sinus such that the "elbow" of the L-shape is positioned directly above the center of the valve, then the anchor catheter **360** could be delivered through the lumen of the guide catheter **362** and out a port at the elbow of the L-shape. A temporary stiffening "stylet" (not shown) could be used through the anchor rail lumen to ensure the anchor is delivered directly downwards to the ideal point at the RV apex.

If any of the previously described anchoring options involving any combination of the RV, SVC, and IVC prove to be undesirable, the coaptation element could instead be anchored directly to the annulus. As shown in FIG. **44**, a series of at least two anchors **370** (similar to the helical RV anchors) could be deployed into the fibrous portion of the annulus, then cables or stabilizing rods **372** could be used to hang or suspend the coaptation element **374** within the annulus plane. Each support cable or rod **372** would need to be relatively taught, so as to prevent motion of the device towards the atrium during systole. Any number of support struts greater than two could be utilized. The support cables for suspending the coaptation element from the annulus could be relatively flexible, and thus the position and mobility of the device would be altered via tension in the cables. Alternatively, the support elements could be relatively stiff to decrease device motion, but this would require changing anchor position to reposition the coaptation element. Although an anchor **376** to the RV apex is shown, the dual annulus anchors **370** might obviate the need for a ventricular anchor.

The general concept of cylindrical stent-based anchor mechanisms for the device could be applied in other structures near the tricuspid valve such as the coronary sinus. For instance, FIG. **45** illustrates an adjustable stabilizing rod **380** mounted on a delivery catheter **382** and secured to an anchor **384** within the coronary sinus. The stabilizing rod **380** attaches via an adjustable sleeve **386** to the catheter **382**, thus suspending the attached coapting element **388** down into the regurgitant orifice. A sliding mechanism on the adjustable sleeve **386** permits adjustment of the length between the coronary sinus anchor **384** and the coaptation device **388**, thus allowing positioning of the coaptation element at the ideal location within the valve plane. For further stability, this coronary sinus anchoring concept could also be coupled with a traditional anchor in the RV apex, as shown.

While venous access to the RV through the subclavian vein and into the superior vena cava is a routine procedure with minimal risk for complications, the fairly flat access

angle of the SVC with respect to the tricuspid valve plane presents a number of challenges for proper orientation of the present coaptation element within the valve. If the catheter were not flexible enough to achieve the correct angle of the coaptation element with respect to the valve plane by purely passive bending, a flex point could be added to the catheter directly proximal to the coaptation element via a pull wire attached to a proximal handle through a double lumen extrusion. For instance, FIG. 46 illustrates an alternative delivery catheter 390 having a pivot joint 392 just above the coapting element 394 for angle adjustment. If a given combination of SVC access angle and/or RV anchor position resulted in a crooked coaptation element within the valve plane, the catheter 390 could be articulated using the pull wire (not shown) until proper alignment is achieved based on feedback from fluoroscopic views.

Additional flex points could be added to further facilitate control of device angle, e.g. another flex point could be added distal to the coaptation element 394 to compensate for the possible case that the RV wall angle (and thus the anchor angle) is skewed with respect to the valve plane. This would require an additional independent lumen within the catheter body 390 to facilitate translation of another pull wire to operate the second flex feature. Alternatively, if a single flex point proximal to the coaptation element were determined to be sufficient for orienting the device, and if the catheter were rigid enough to resist the forces of systolic flow, the section 396 of the device distal to the coaptation element could be removed all together. This would leave only one anchoring point for the device in the SVC or subcutaneously to the subclavian vein. Also, as an alternative to an actively-controlled flex point, the catheter could contain a shape-set shaft comprised of Nitinol or another shape memory material, which would be released from a rigid delivery sheath into its "shaped" form in order to optimize device angle from the SVC. It could be possible to have a few catheter options of varying pre-set angles, yet choose only one after evaluation of the SVC-to-valve plane angle via angiographic images.

Instead of using an active mechanism within the catheter itself to change its angle, another embodiment takes advantage of the surrounding anatomy, i.e. the SVC wall. FIGS. 47A and 47B show two ways to anchor the delivery catheter 400 to the superior vena cava SVC for stabilizing a coapting element 402. For example, a variety of hooks or anchors 404 could extend from a second lumen within the catheter 402 with the ability to grab onto the SVC wall and pull the catheter in that direction (FIGS. 47A and 47B). Alternatively, a stiffer element could extend outwards perpendicular to the catheter axis to butt up against the SVC wall and push the catheter in the opposite direction. For especially challenging SVC geometries, such a mechanism could potentially be useful for achieving better coaxial alignment with the valve.

FIGS. 48A and 48B show an active regurgitation reduction device 410 having pull wires 412 extending through the delivery catheter 414 for altering the position of the coapting element 416 within the tricuspid valve leaflets. If the coapting element 416 is located out of the middle of the valve leaflets such that it does not effectively plug any regurgitant jets, which can be seen on echocardiography, then one of the pull wires 412 can be shortened or lengthened in conjunction with rotating the catheter 414 to reposition the coapting element 416, such as seen from FIG. 48A to FIG. 48B.

Although pacemaker leads are frequently anchored in the right ventricle with chronic success, the anchor for the present device would see significantly higher cyclic loads

due to systolic pressure acting on the coaptation element. Given that the right ventricle wall can be as thin as two millimeters near the apex and the tissue is often highly friable in patients with heart disease, anchoring a device in the ventricle may not be ideal. An alternative anchoring approach could take advantage of the fairly collinear orientation of the superior and inferior vena cava, wherein, as seen in FIG. 49, two stent structures 420, 422 would effectively "straddle" the tricuspid valve by expanding one in the superior vena cava and the other in the inferior vena cava. The coaptation element 424 would then hang down through the tricuspid valve plane from an atrial shaft 426 attached to a connecting wire or rod 428 between the two caval stents 420, 422. In order to resist motion of the coaptation element under systolic forces, the shaft 426 from which the coaptation element 424 hangs would be fairly rigid under compressive and bending stresses. The coaptation element 424 would desirably be positioned within the valve using a sliding mechanism along the connecting rod 428 between the two caval stents.

The coaxial orientation of the SVC and IVC could also be leveraged for delivering an anchor into the RV. A delivery catheter could be passed through the SVC into the IVC, and a "port" or hole off the side of the delivery catheter could be aligned with the center of the valve. At this point, the anchor could be passed through the lumen of the delivery system and out the port, resulting in a direct shot through the center of the annulus and to the RV wall in the ideal central anchor location.

This concept could potentially be applied to the left side of the heart as well, to address mitral regurgitation. A coaptation element could reside between the mitral valve leaflets with anchors on both the proximal and distal ends: one attaching to the septal wall, and the other anchoring in the left atrial appendage. The septal anchor could be a helical or hook-style anchor, whereas the left atrial appendage anchor could be an expandable metallic structure with a plurality of struts or wireforms designed to oppose against the appendage wall and provide stability to the coaptation element.

Pacemaker leads frequently lead to tricuspid regurgitation (TR) by pinning a leaflet or interfering with leaflet mobility. In this particular embodiment, a device, a gap filler, is designed to be introduced over the offending pacemaker lead (of course, applicable also to those with organic tricuspid regurgitation and a pacemaker lead in place). The invention is a tricuspid regurgitant volume gap filler that is placed over the existing pacemaker lead via a coil wound over the lead or a slit sheath approach, which acts like a monorail catheter. The gap filler catheter is advanced over the pacemaker lead and the tricuspid regurgitation is evaluated by echo while the monorail gap filler device is placed into the regurgitant orifice. The proximal end of the gap filler allows for crimping and truncating the catheter post-balloon inflation or gap filler deployment. This mates the monorail gap filler to the pacemaker lead at the proper position within the tricuspid valve.

FIGS. 50-51 are schematic views of a coapting element 430 mounted for lateral movement on a flexible delivery catheter 432 that features controlled buckling. It is challenging to reposition the coaptation element 430 from an off-center location to the ideal central location within the valve plane, given a fixed angle from the SVC and a fixed anchor position in the RV. The device catheter 432 could be comprised of a fairly stiff shaft except for two relatively flexible regions 434, 436 directly proximal and distal to the coaptation element section. The farthest distal section of the

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coaptation catheter 432 could be locked down relative to the anchor rail over which it slides, and then the catheter 432 could be advanced distally thus compressing it and causing the two flexible sections 434, 436 to buckle outwards and displace the coaptation element laterally with respect to the catheter axis (see FIG. 50C). At this point, the user could employ a combination of sliding and rotating of the catheter to reposition the coaptation element 430 within the valve using short-axis echo feedback. Instead of locking the distal end of the catheter onto an anchor rail before adjustment, if the catheter were comprised of multiple lumens, the outer lumen could slide distally relative to the inner lumen, thus producing the same buckling effect.

In another embodiment, not shown, an alternative approach could be to rely on the contractile motion of the heart to move a tapered coaptation element in and out of the tricuspid valve plane. A tapered coaptation element, with a smaller cross-section proximally (towards the atrium) and larger cross-section distally (towards the ventricle), would be attached to a rigid distal railing and anchor. During systolic contraction, the anchor and therefore the attached coaptation element would move towards the annulus, thus allowing the tricuspid leaflets to coapt around the larger cross-section of the device. Conversely, diastolic expansion of the RV would bring the anchor and therefore the coaptation element downwards such that the smaller cross-section of the device is now within the annulus plane, thus minimizing diastolic stenosis. A combination of a tapered element with a spring could be used if RV wall motion towards the annulus is not sufficient to move the device.

While the foregoing is a complete description of the preferred embodiments of the invention, various alternatives, modifications, and equivalents may be used. Moreover, it will be obvious that certain other modifications may be practiced within the scope of the appended claims.

What is claimed is:

1. An implantable heart valve coaptation system for reducing regurgitation through the valve, comprising the following implantable elements:

an elongated flexible rail having a ventricular anchor on the distal end thereof adapted to anchor into tissue within a ventricle, wherein the flexible rail has a length sufficient to extend from the ventricular anchor in the ventricular tissue to a subclavian vein, the flexible rail being made of material suitable for implant in the human body;

a delivery catheter having a lumen through which the flexible rail passes, the delivery catheter being made of material suitable for implant in the human body;

a valve leaflet coaptation member fixed on a distal end of the delivery catheter having a bell-shaped cover with a first end open and a flexible inner support holding the first end open, the delivery catheter having a length sufficient to extend from the coaptation member positioned within the heart valve leaflets to the subclavian vein, the coaptation member being made of material suitable for implant in the human body; and

a locking collet on a proximal end of the delivery catheter for securing the axial position of the coaptation member and delivery catheter on the flexible rail, the locking collet being made of material suitable for implant in the human body, the locking collet and/or catheter being adapted to be subcutaneously anchored outside the subclavian vein.

2. The system of claim 1, wherein the locking collet includes a pair of internally threaded tubular grips each fixed to one of two separate sections of the delivery catheter and

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engaging a common externally threaded tubular shaft member, and act on a wedge member interposed between at least one of the grips and the flexible rail to securing the axial position of the coaptation member and delivery catheter on the flexible rail.

3. The system of claim 1, wherein the first end of the bell-shaped cover of the coaptation member is on a distal or ventricular side thereof.

4. The system of claim 3, wherein the second end of the bell-shaped cover has flow through openings.

5. The system of claim 1, wherein the flexible inner support comprises a flexible frame with struts emanating from a central collar and engaging the first end of the bell-shaped cover.

6. The system of claim 1, wherein the flexible inner support comprises a flexible frame with struts that extend substantially the length of the bell-shaped cover.

7. The system of claim 1, wherein the flexible inner support comprises a compressible foam member substantially filling the cover.

8. The system of claim 1, wherein the cover is formed of polycarbonate urethane.

9. An implantable heart valve coaptation system for reducing regurgitation through the valve, comprising the following implantable elements:

an elongated flexible rail having a ventricular anchor on the distal end thereof adapted to anchor into tissue within a ventricle, wherein the flexible rail has a length sufficient to extend from the ventricular anchor in the ventricular tissue to a subclavian vein, the flexible rail being made of material suitable for implant in the human body;

a delivery catheter having a lumen through which the flexible rail passes, the delivery catheter being made of material suitable for implant in the human body;

a valve leaflet coaptation member fixed on a distal end of the delivery catheter having a smooth outer cover with a compressible foam inner support, the delivery catheter having a length sufficient to extend from the coaptation member positioned within the heart valve leaflets to the subclavian vein, the coaptation member being made of material suitable for implant in the human body; and

a locking collet on a proximal end of the delivery catheter for securing the axial position of the coaptation member and delivery catheter on the flexible rail, the locking collet being made of material suitable for implant in the human body, the locking collet and/or catheter being adapted to be subcutaneously anchored outside the subclavian vein.

10. The system of claim 9, wherein the ventricular anchor comprises two separate anchors that cooperate to secure the flexible rail of the flexible rail to the ventricle tissue.

11. The system of claim 9, wherein the coaptation member is fixed over a section of the catheter having perforations opening to a lumen of the catheter.

12. The system of claim 11, wherein the cover provides a closed chamber around the perforations.

13. The system of claim 11, wherein the compressible foam member substantially fills the cover and is an open cell foam that permits blood flow therethrough.

14. The system of claim 13, wherein the flexible inner support further comprises a flexible frame with struts that extend substantially the length of the cover between the compressible foam member and the cover.

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15. An implantable heart valve coaptation system for reducing regurgitation through the valve, comprising the following implantable elements:

an elongated flexible rail having a ventricular anchor on the distal end thereof adapted to anchor into tissue within a ventricle, wherein the flexible rail has a length sufficient to extend from the ventricular anchor in the ventricular tissue to a subclavian vein, the flexible rail being made of material suitable for implant in the human body;

a delivery catheter having a lumen through which the flexible rail passes, the delivery catheter being made of material suitable for implant in the human body;

a valve leaflet coaptation member fixed on a distal end of the delivery catheter over a section of the catheter having perforations opening to a lumen of the catheter, the coaptation member having an outer cover of polycarbonate urethane with a flexible inner support holding the cover outward from the delivery catheter, the outer cover providing a closed chamber around the perforations, and wherein the delivery catheter has a length sufficient to extend from the coaptation member positioned within the heart valve leaflets to the subclavian vein, the coaptation member being made of material suitable for implant in the human body; and

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a locking collet on a proximal end of the delivery catheter for securing the axial position of the coaptation member and delivery catheter on the flexible rail, the locking collet being made of material suitable for implant in the human body, the locking collet and/or catheter being adapted to be subcutaneously anchored outside the subclavian vein.

16. The system of claim 15, wherein the cover is a polycarbonate urethane both ends being closed by being heat bonded to the catheter.

17. The system of claim 15, wherein the cover is bell-shaped with both ends secured to the catheter.

18. The system of claim 17, wherein the cover is a polycarbonate urethane with both ends heat bonded to the catheter.

19. The system of claim 15, wherein the flexible inner support comprises a compressible foam member substantially filling the cover.

20. The system of claim 15, wherein the flexible inner support comprises a flexible frame with struts emanating from a central collar and engaging the inside of the cover.

21. The system of claim 15, wherein the flexible inner support comprises a flexible frame with struts that extend substantially the length of the cover.

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